

■ 3D Near-infrared Imaging Based on a Single-photon Avalanche Diode Sensor

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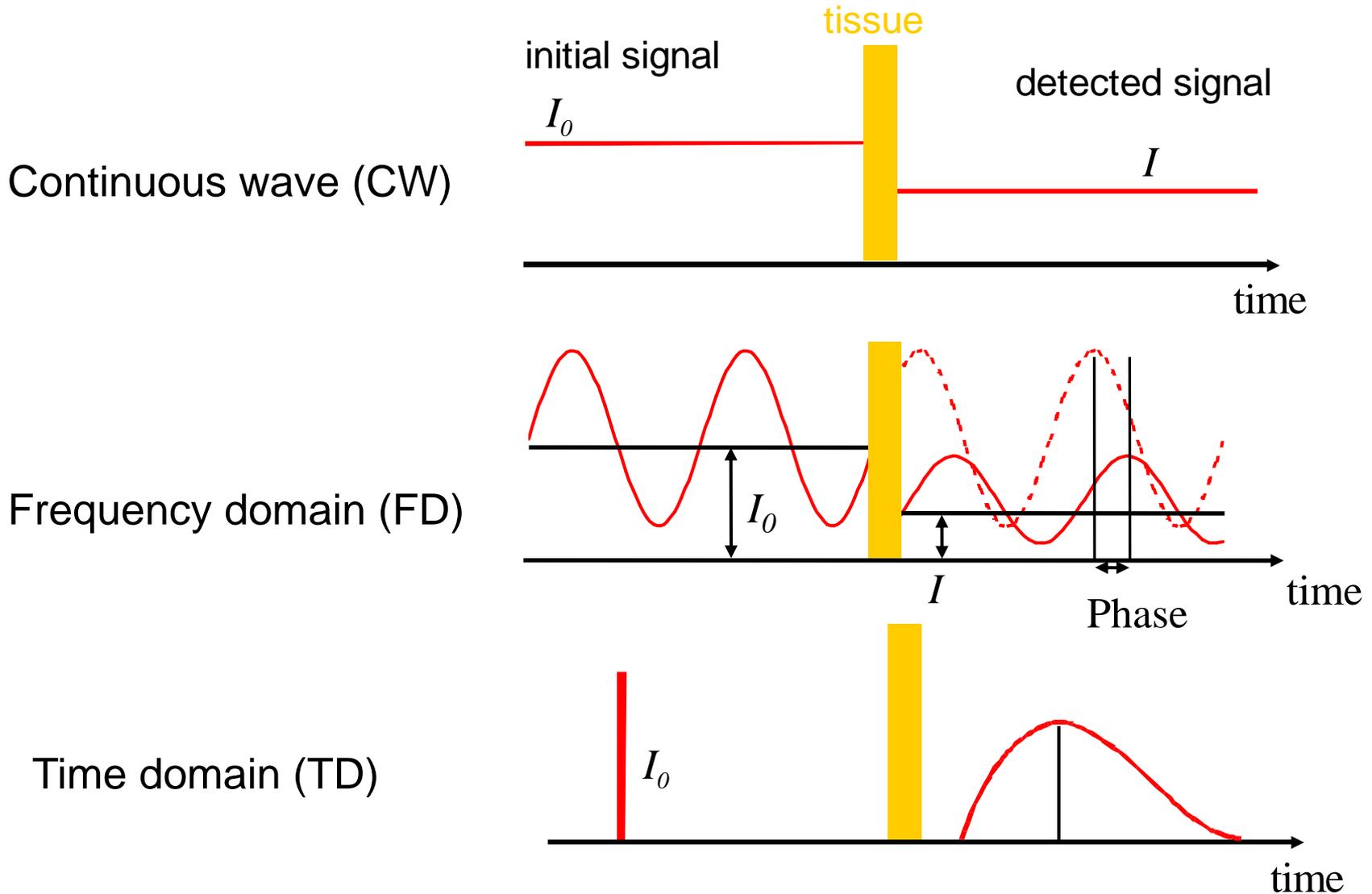
Edoardo Charbon



ÉCOLE POLYTECHNIQUE
FÉDÉRALE DE LAUSANNE



Experimental Techniques

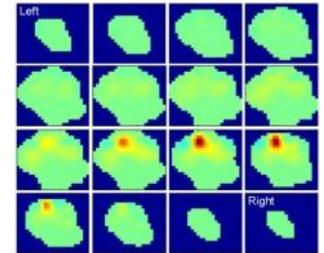


Near Infrared Imaging (NIRI)

- Low spatial resolution (~1cm resolution)
- 3D images require long acquisition times
- CW systems can be miniaturized
- TD and FD systems are bulky
- Low number of sources/detectors

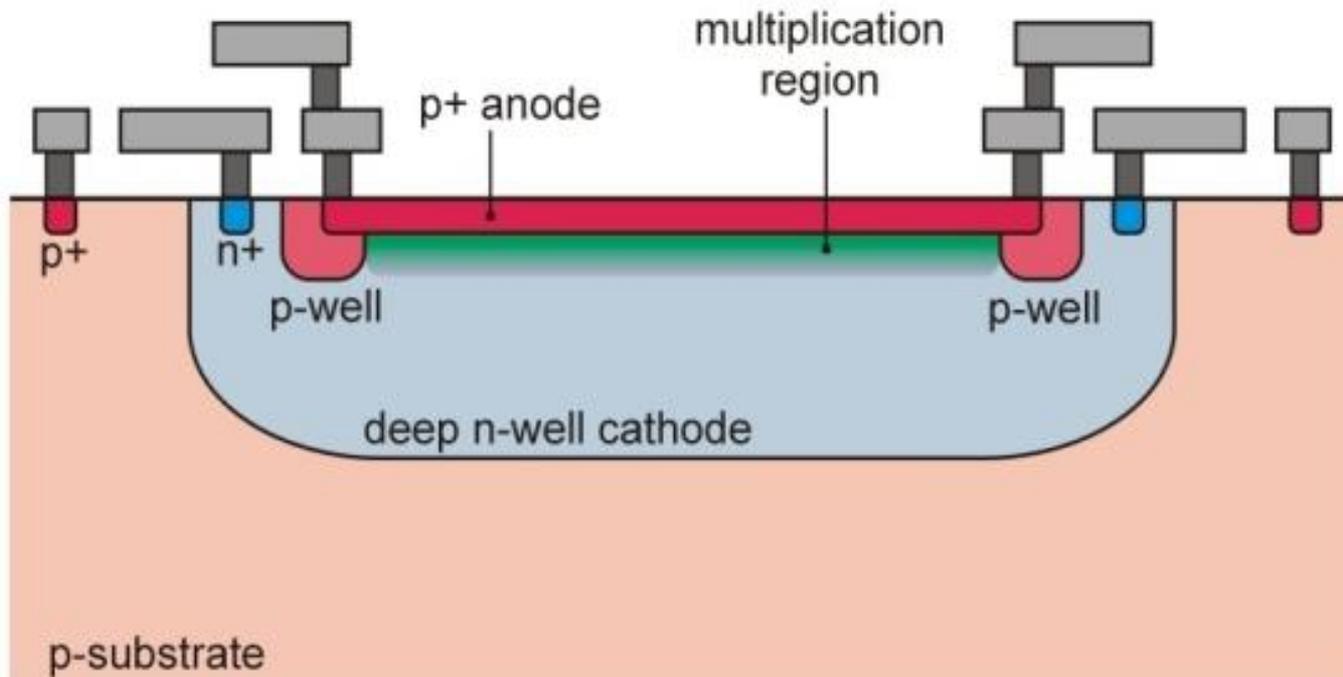


[Muehleemann T *et al* Opt. Express 2008]



[Wells K *et al* Proc. SPIE 1997]

Single-photon avalanche diode (SPAD)

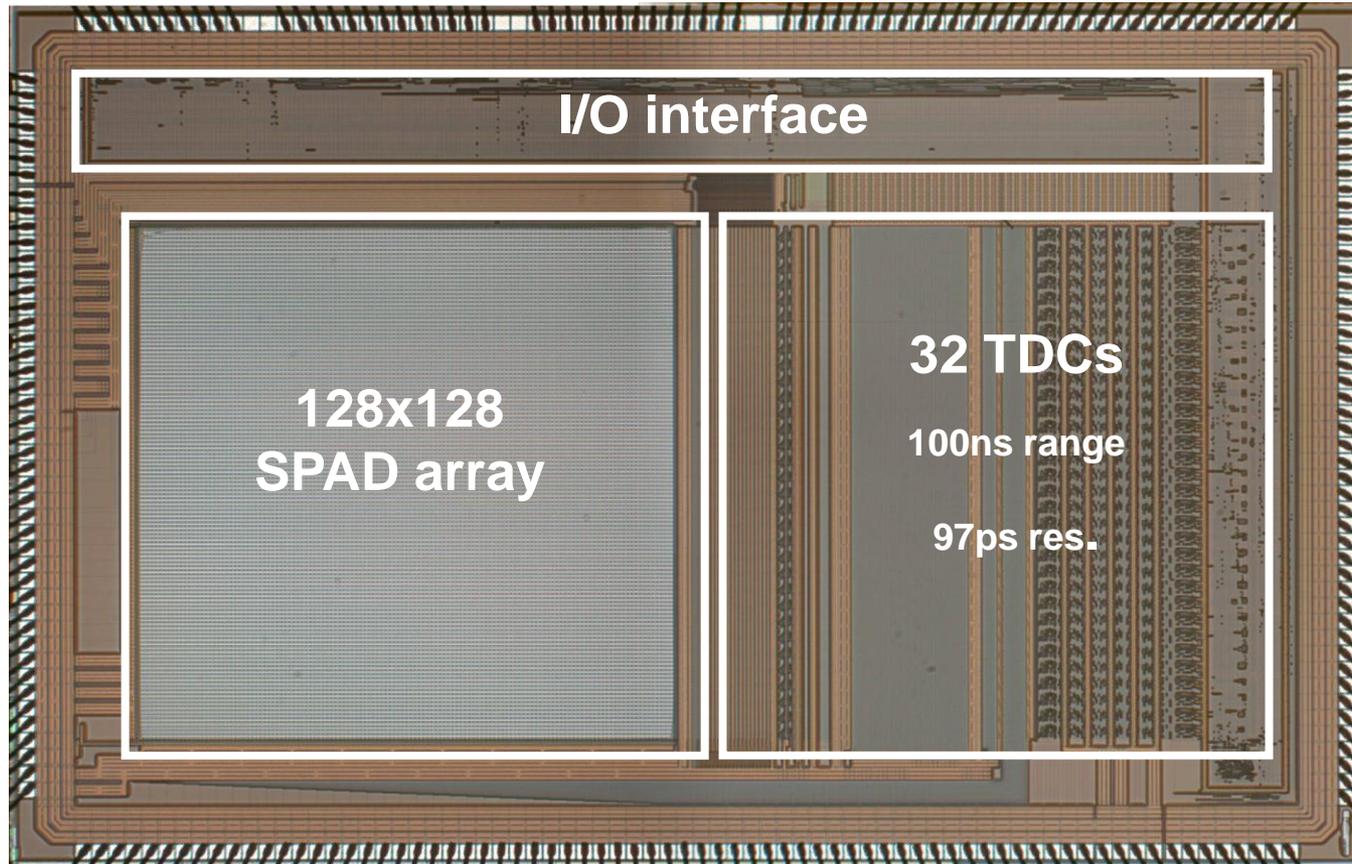


Objective

- New 3D NIRI system:
 - High resolution images: <1cm
 - Almost real time operation
 - Bedside applicable

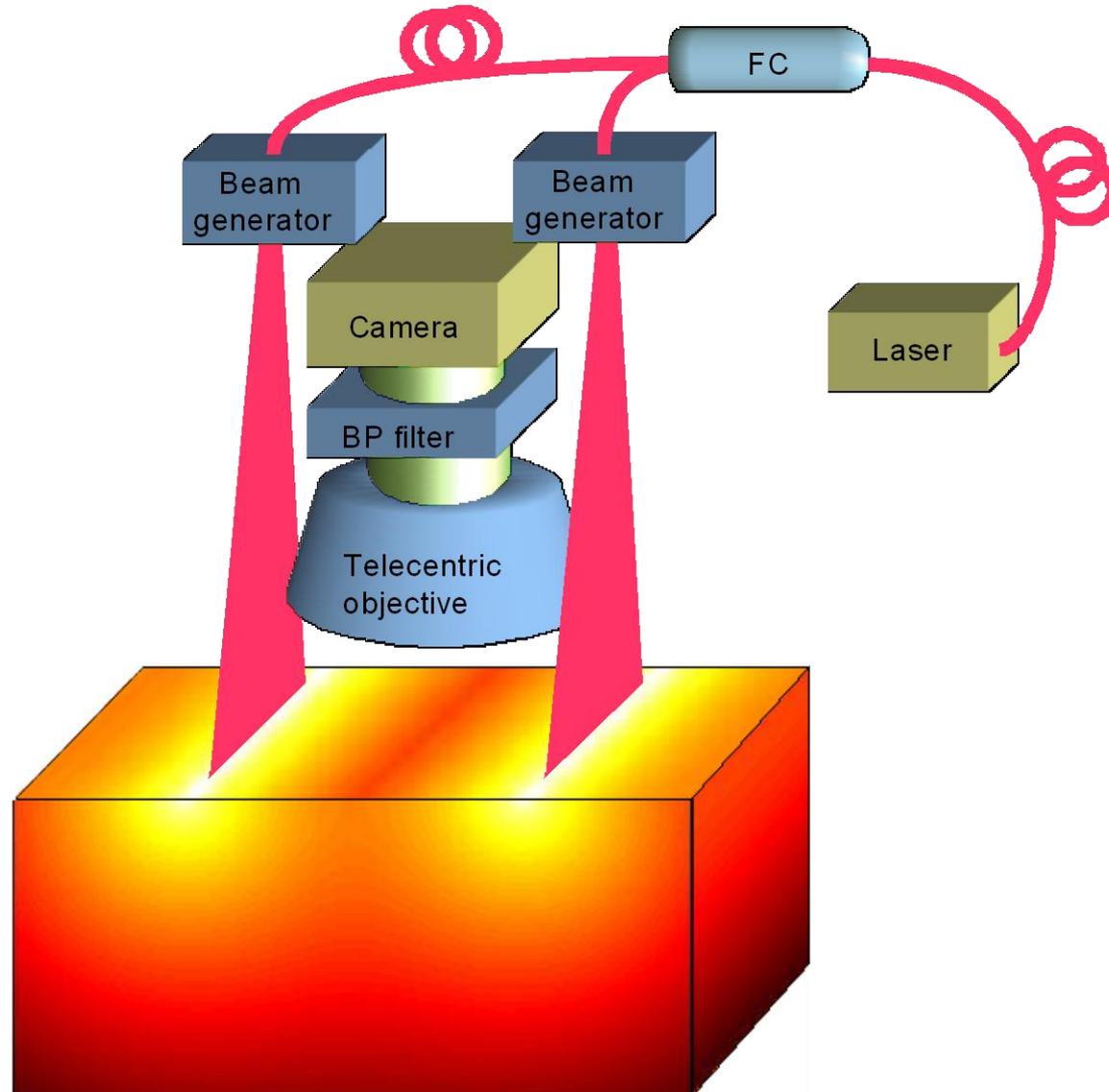
- SPAD imagers offer:
 - High resolution images
 - Time resolved measurements

SPAD Image Sensor: LASP Chip

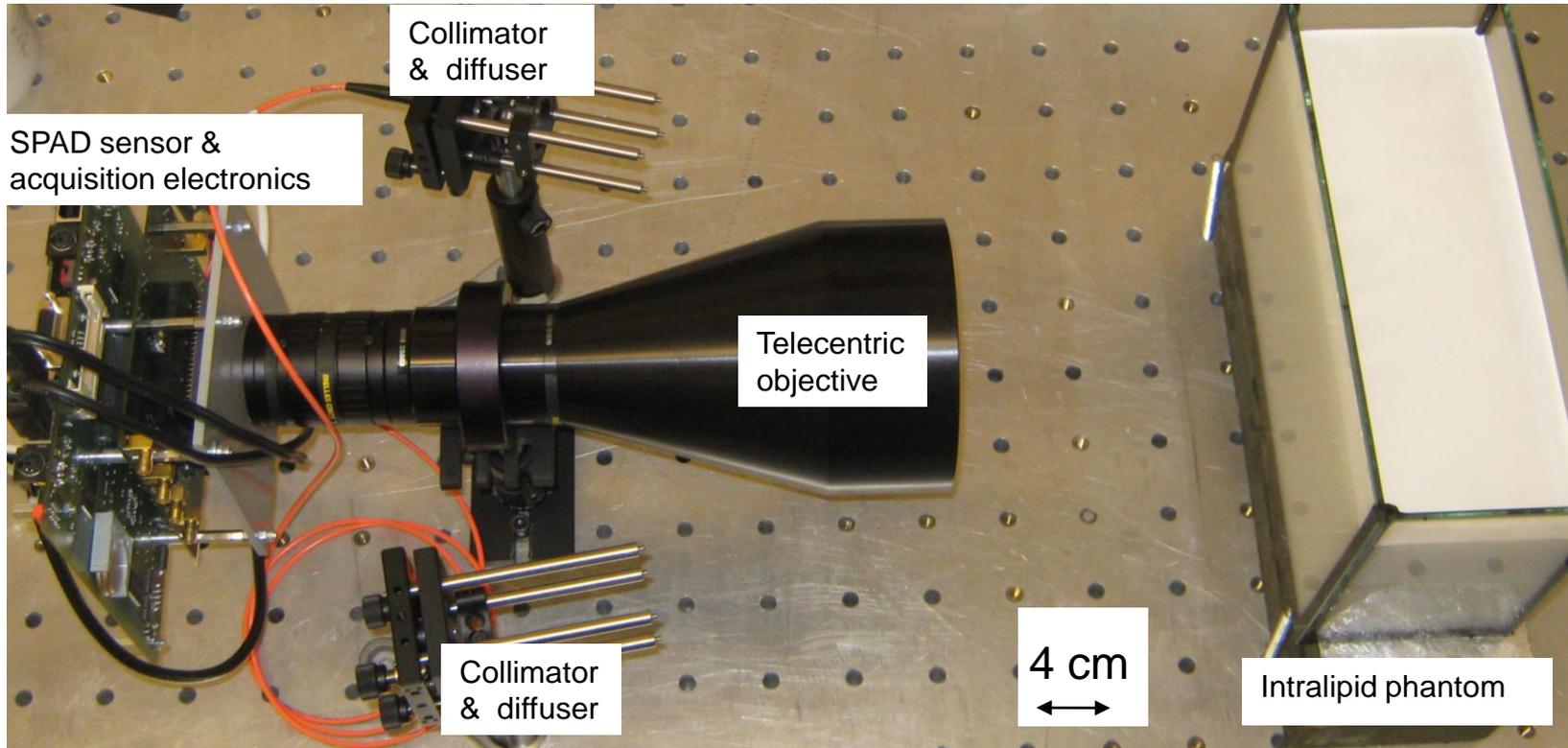


[Niclass *et al* JSSC 2008]

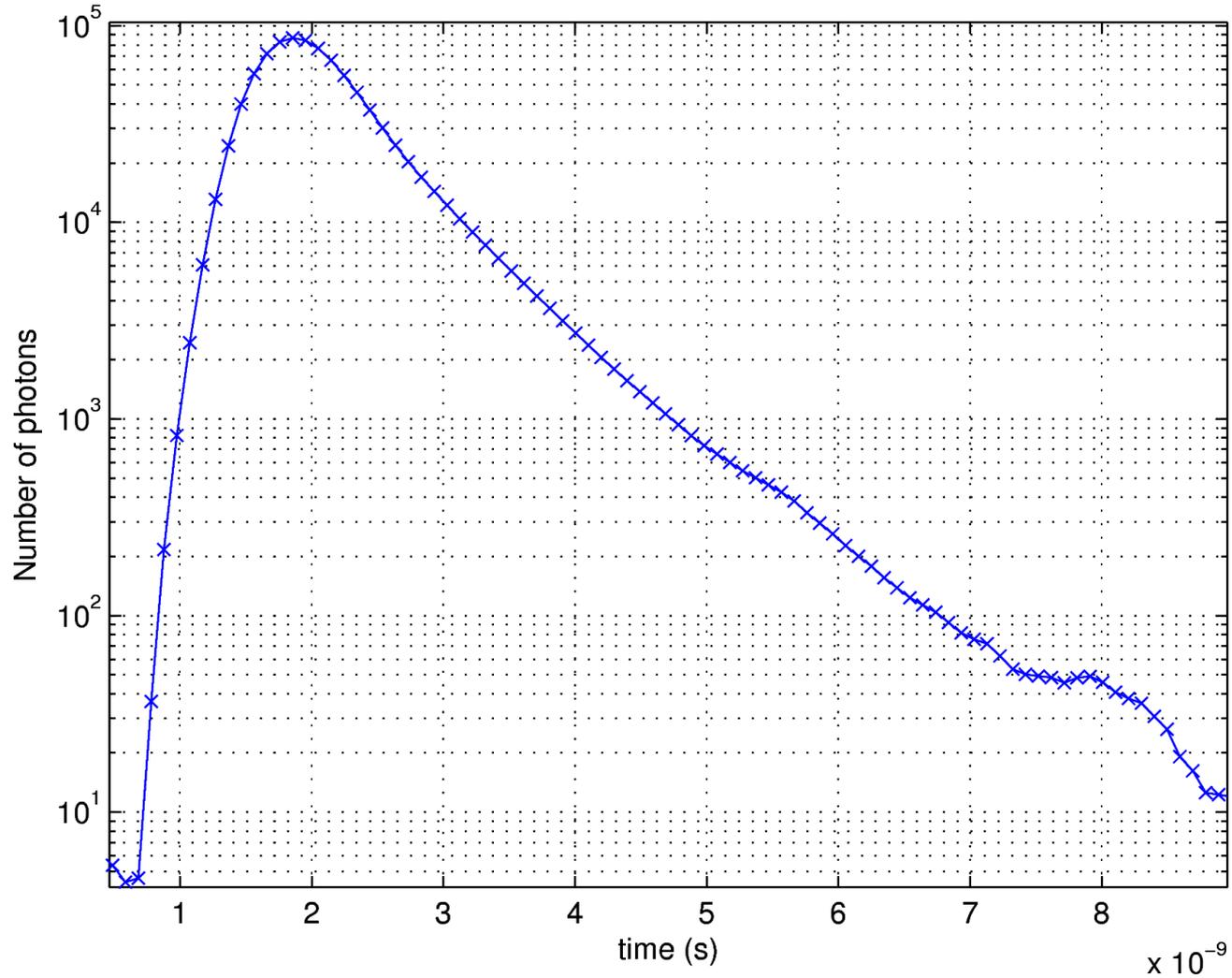
Experimental Setup with Cylindrical Waves I



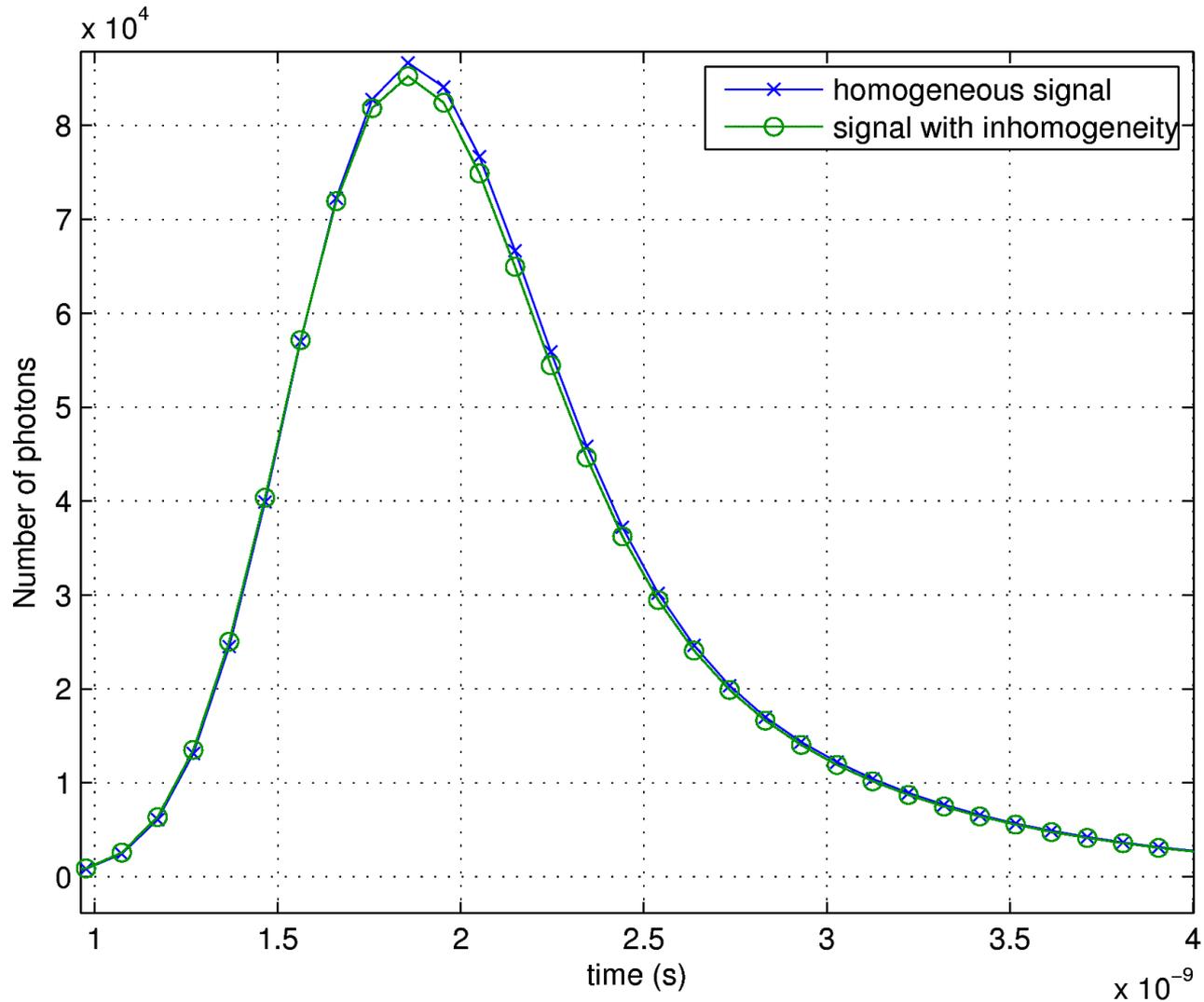
Experimental Setup with Cylindrical Waves II



Phantom Measurements I



Phantom Measurements II



The Diffusion Equation

- Homogeneous medium
- Fourier in the time domain
- Born approximation

Object to be reconstructed

$$\nabla^2 + k^2 \tilde{U}_s(\mathbf{r}, \omega_t) = O(\mathbf{r}) \tilde{U}_0(\mathbf{r}, \omega_t)$$

Measurement

Photon density in the homogeneous medium

Object to be reconstructed

$$U_s(\mathbf{r}, \omega_t) = - \iiint G(\mathbf{r}, \mathbf{r}', \omega_t) O(\mathbf{r}') U_0(\mathbf{r}', \omega_t) d\mathbf{r}'$$

Measurement

Matrix coefficients

Fourier in the X dimension

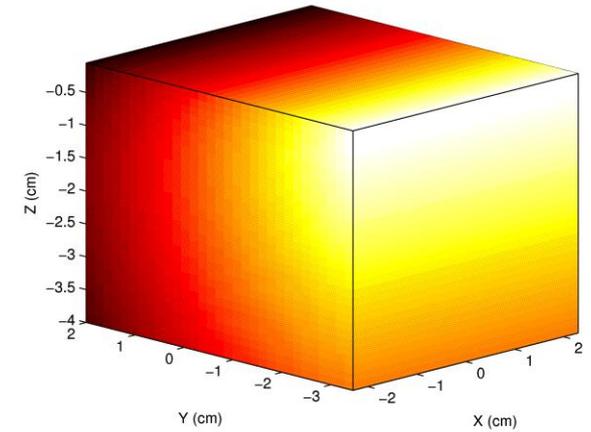
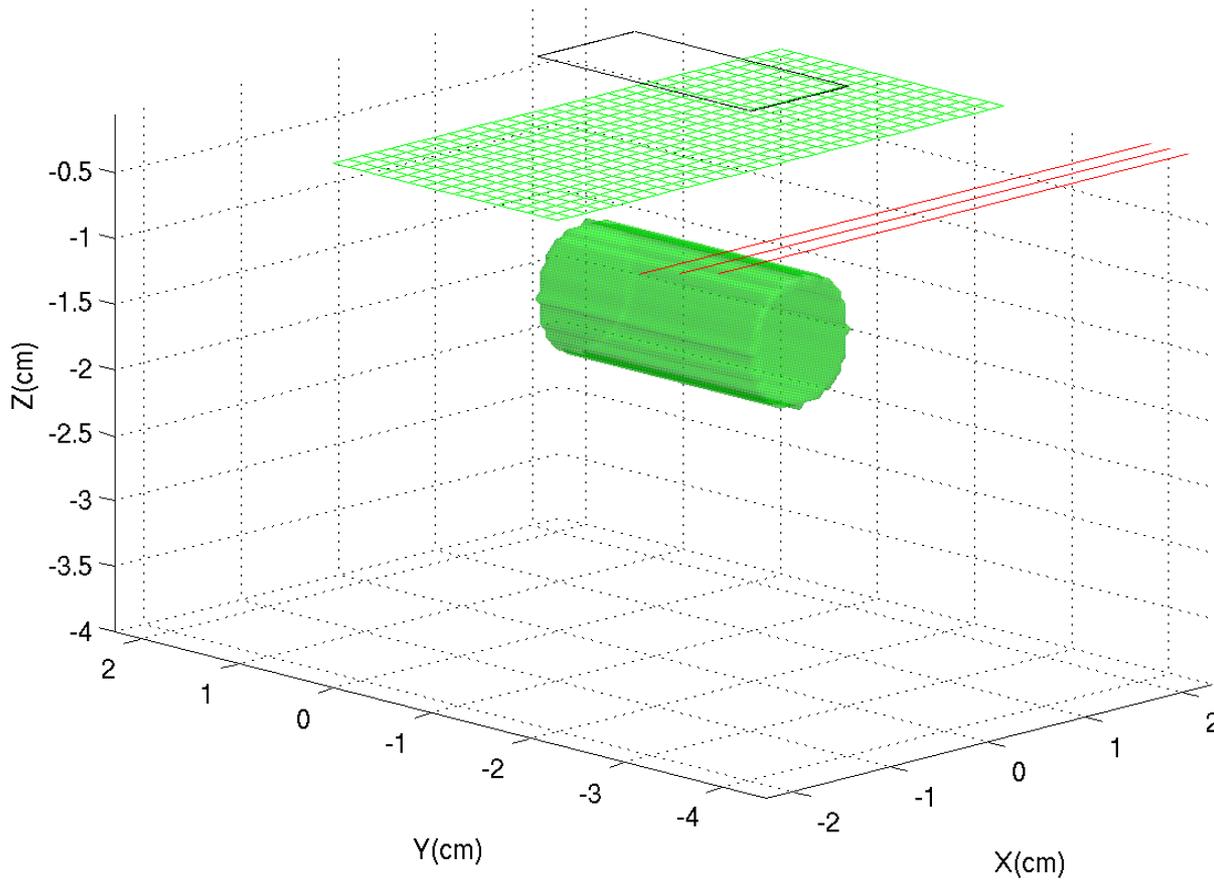
$$\left(\nabla_{yz}^2 + k^2 - w_x^2 \right) \tilde{U}_s(\mathbf{r}_{yz}, \omega_x, \omega_t) = F_x \left(O(\mathbf{r}') \tilde{U}_0(\mathbf{r}', \omega_t) \right)$$

X independent

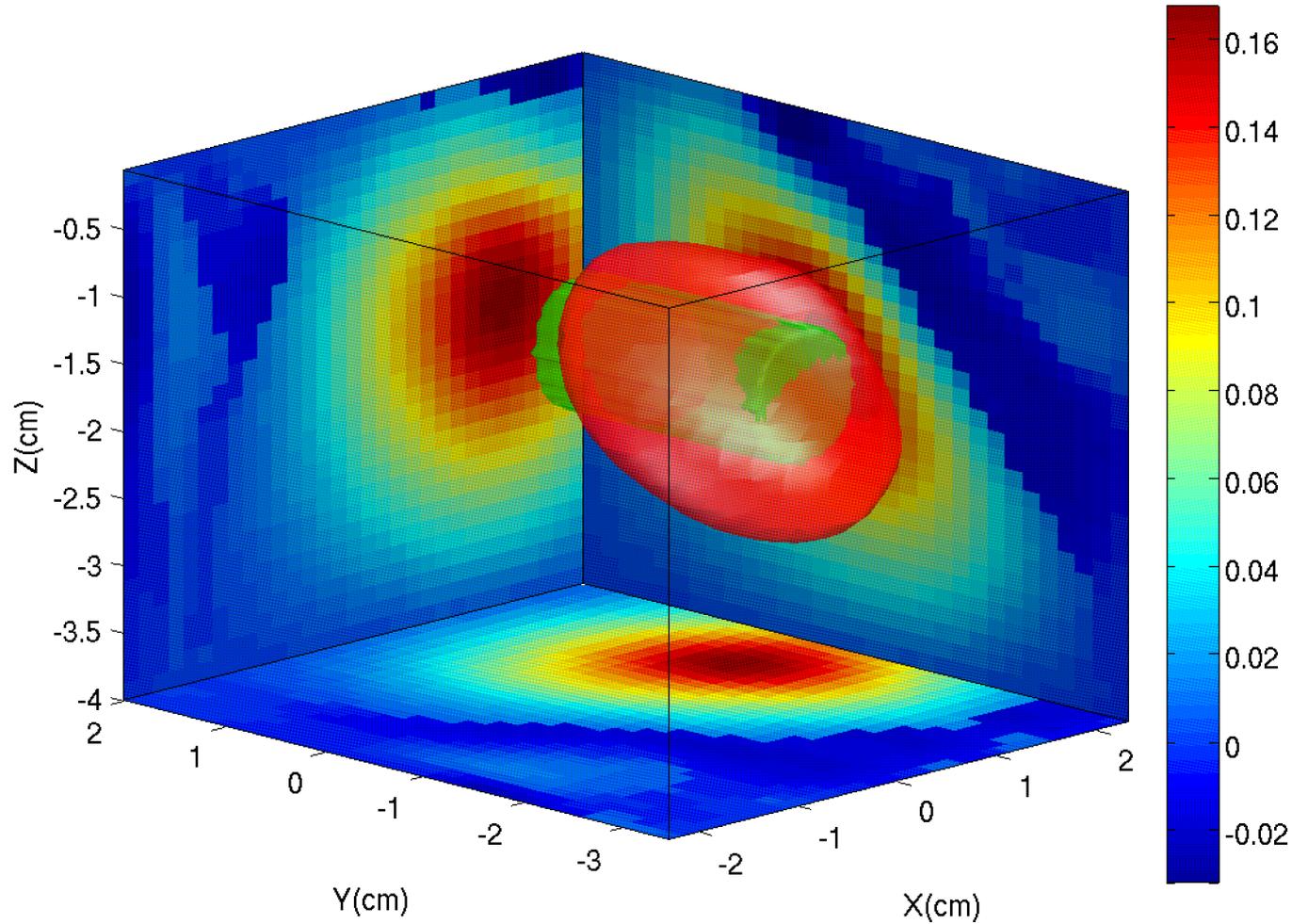
The triple integral is reduced to a double integral

$$U_s(\mathbf{r}_{yz}, \omega_x, \omega_t) = - \iint G(\mathbf{r}_{yz}, \mathbf{r}'_{yz}, \omega_x, \omega_t) O(\mathbf{r}'_{yz}, \omega_x) U_0(\mathbf{r}'_{yz}, \omega_t) d\mathbf{r}'_{yz}$$

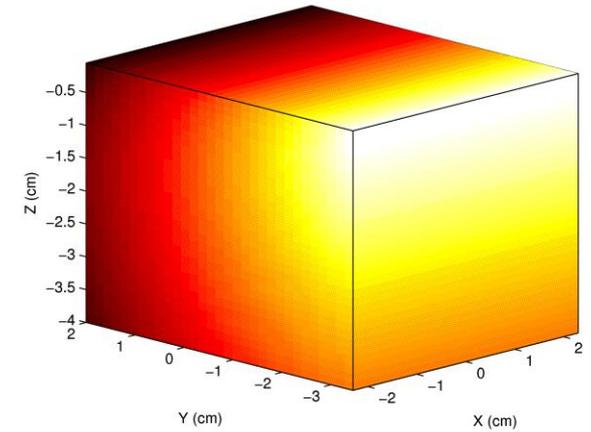
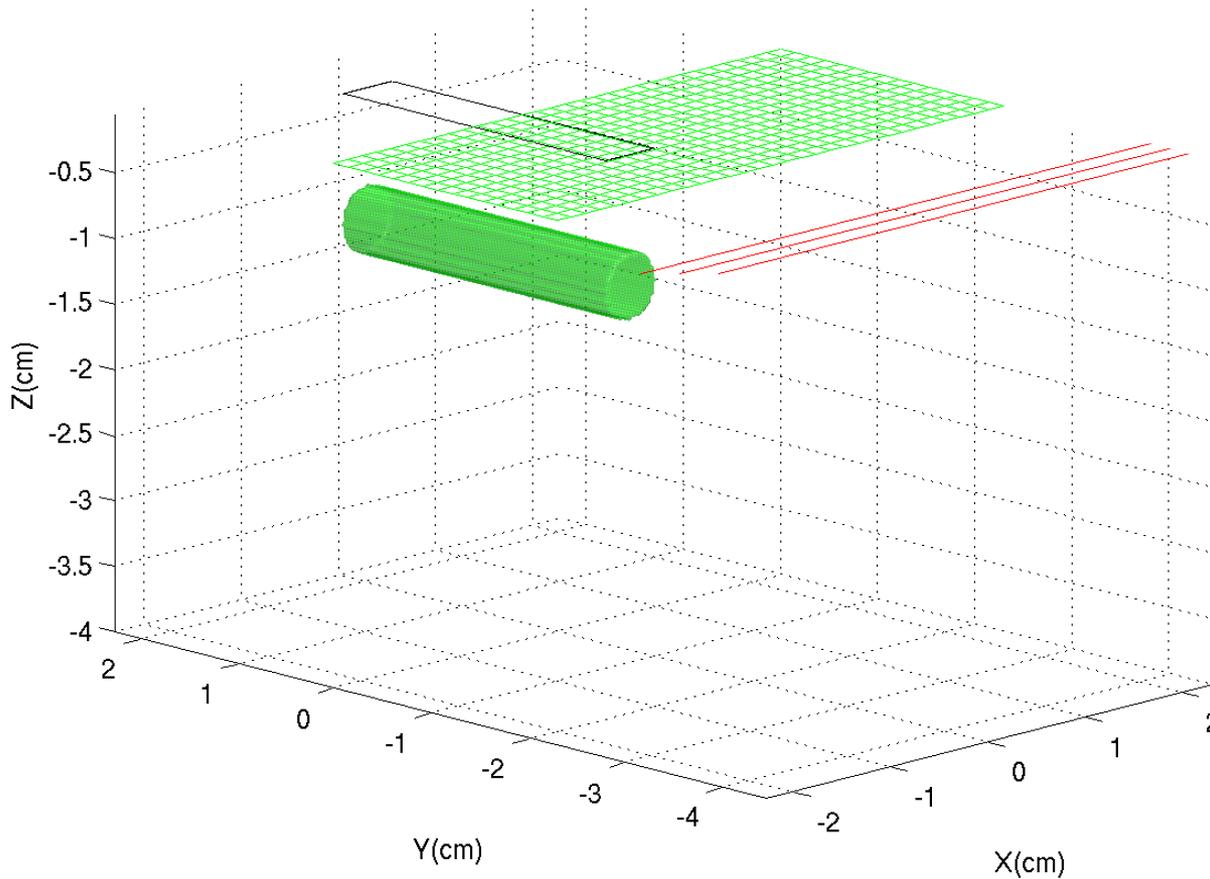
Experimental Results: Setup 1



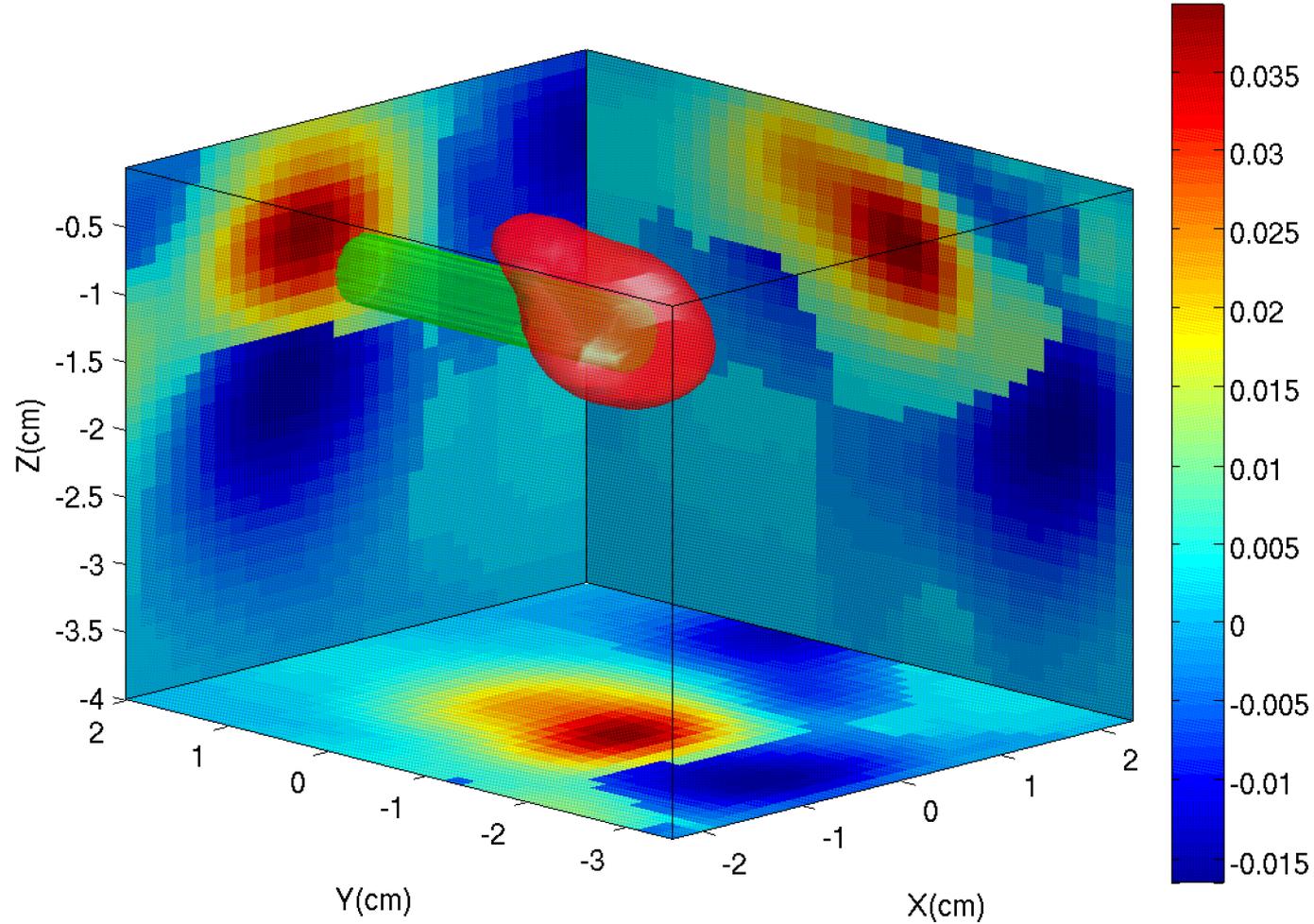
Experimental Results: Reconstruction 1



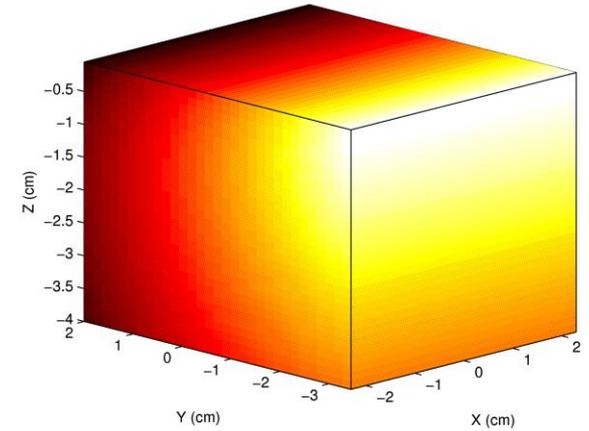
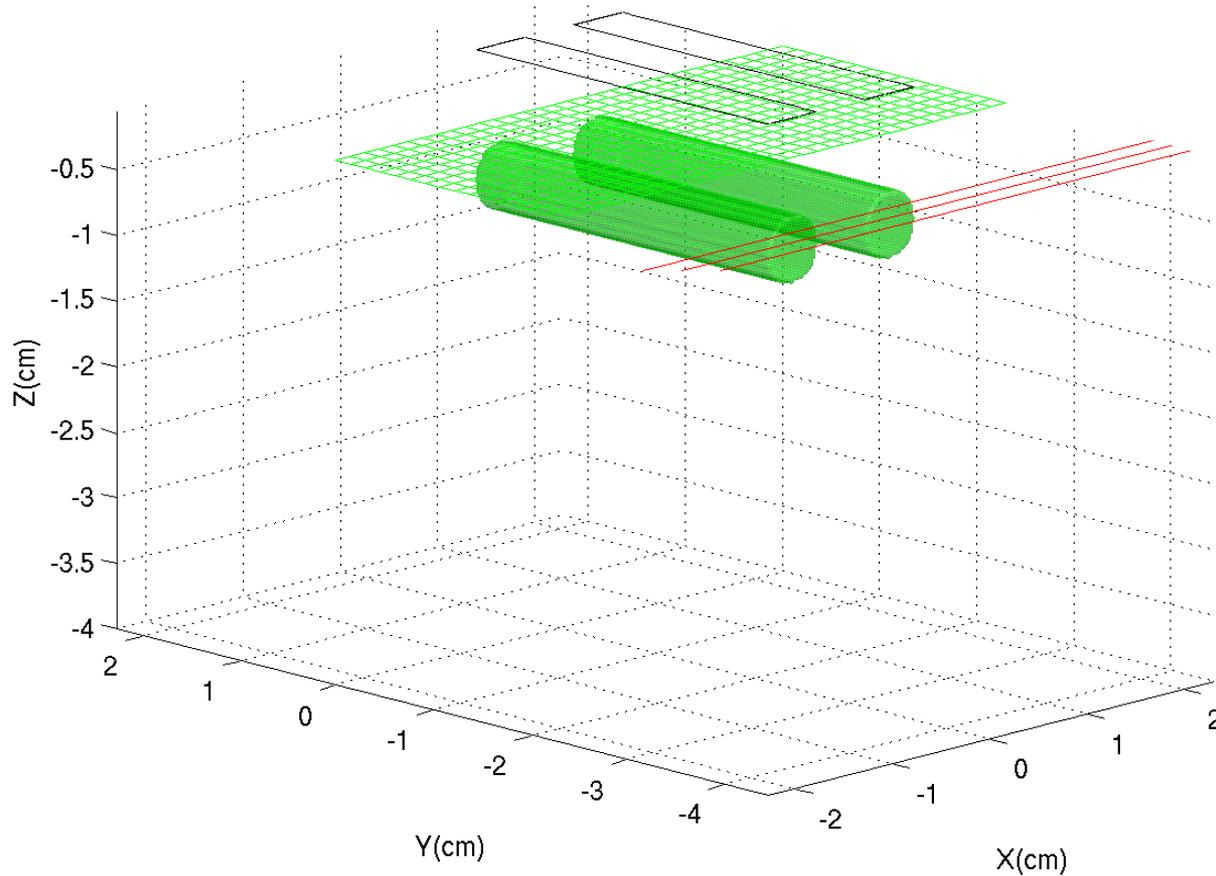
Experimental Results: Setup 2



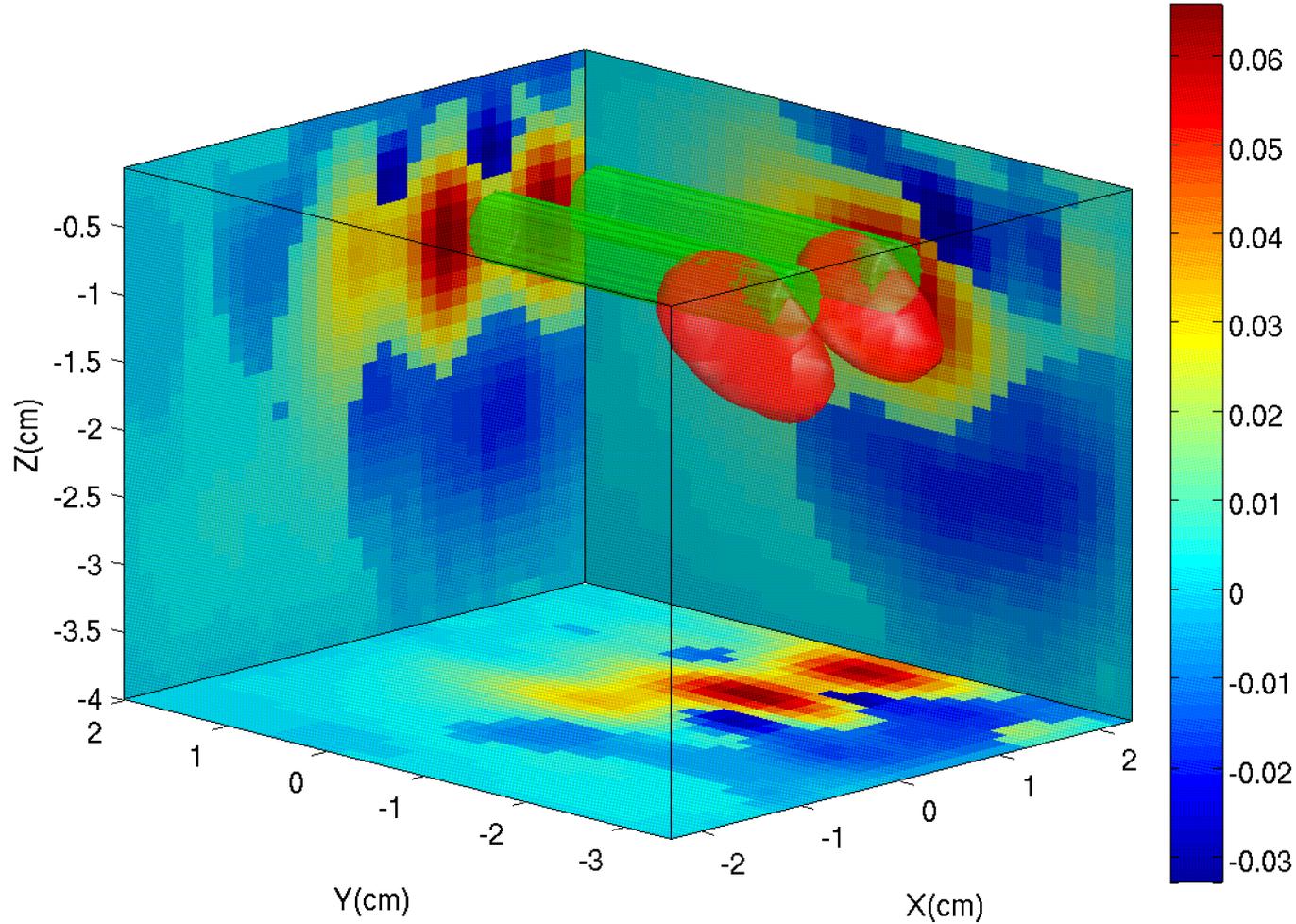
Experimental Results: Reconstruction 2



Experimental Results: Setup 3



Experimental Results: Reconstruction 3



Summary & Outlook

- SPADs imagers make possible time-resolved high spatial resolution measurements for 3D NIRI
 - ✓ Design a NIRI system based on a SPAD image sensor
 - ✓ Develop the image reconstruction algorithm
 - ✓ Build the system
 - ➔ Performance evaluation
 - Design a new SPAD image sensor
 - Pre-clinical trials

Thanks to

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Martin Frenz

■ Questions ?



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University Hospital Zurich | Clinic of Neonatology



UniversitätsSpital
Zürich



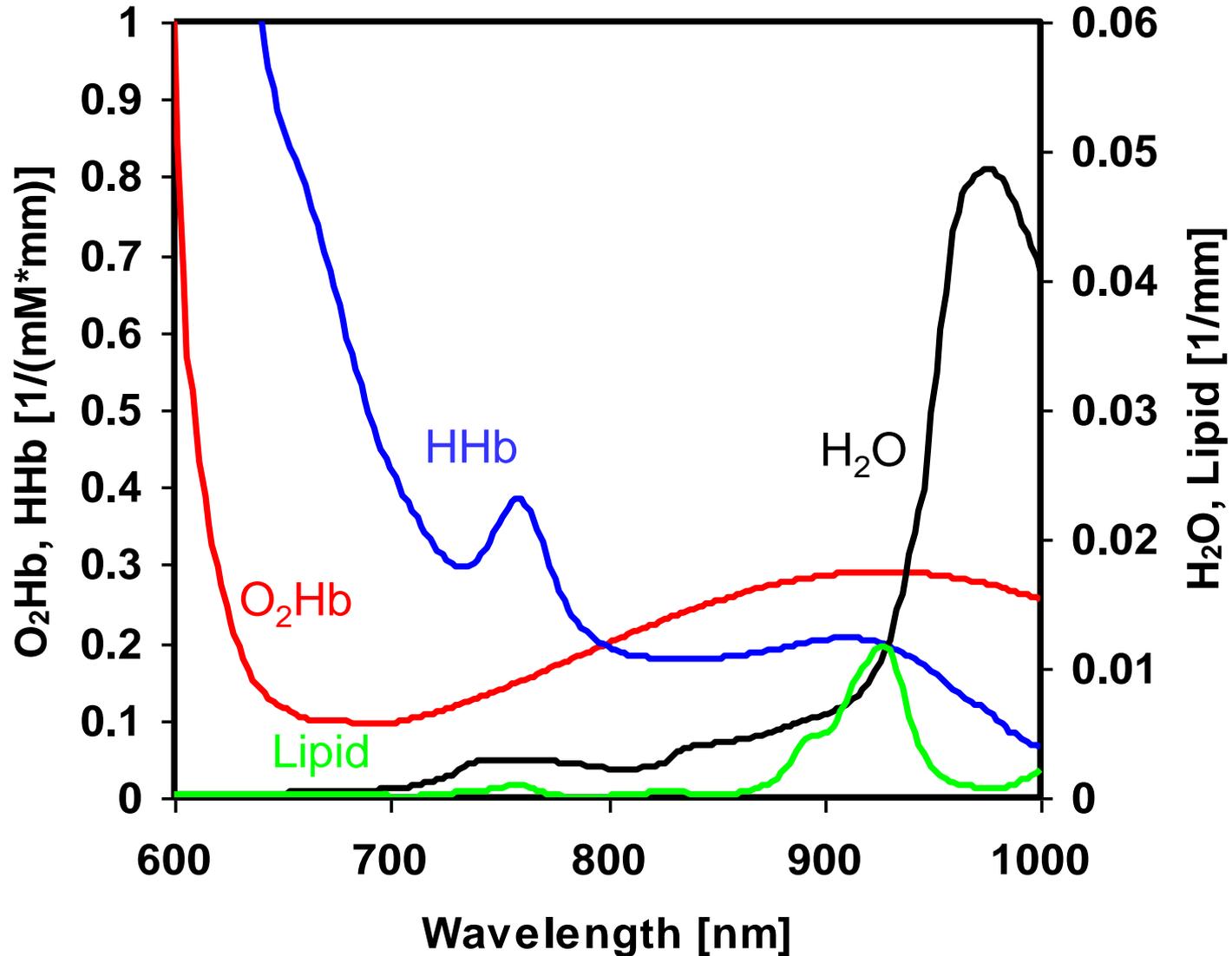
Dept. Frauenheilkunde
Klinik für Neonatologie



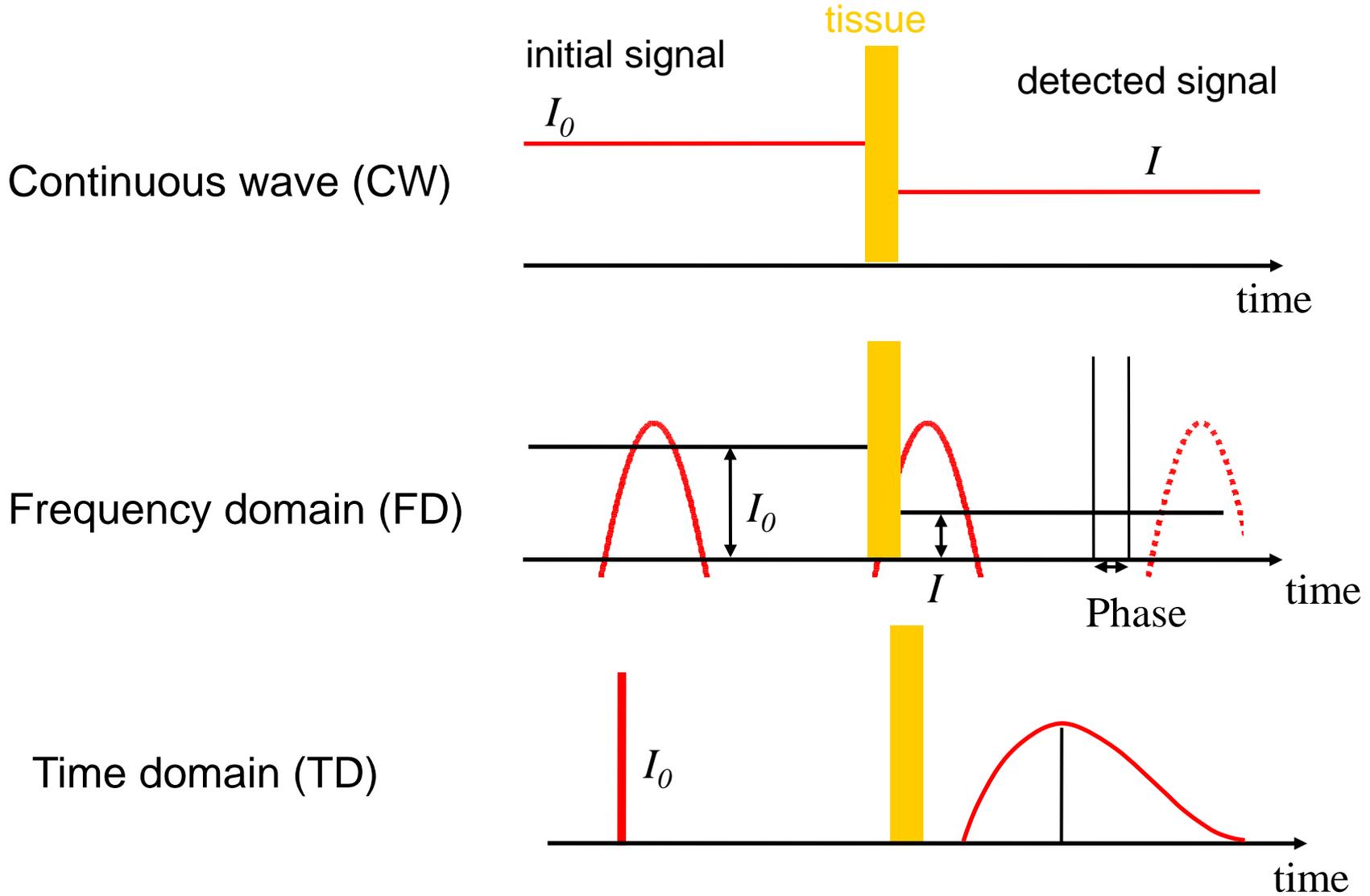
Outline

- Introduction
- Imaging system
- Image reconstruction
- Preliminary results

Absorption

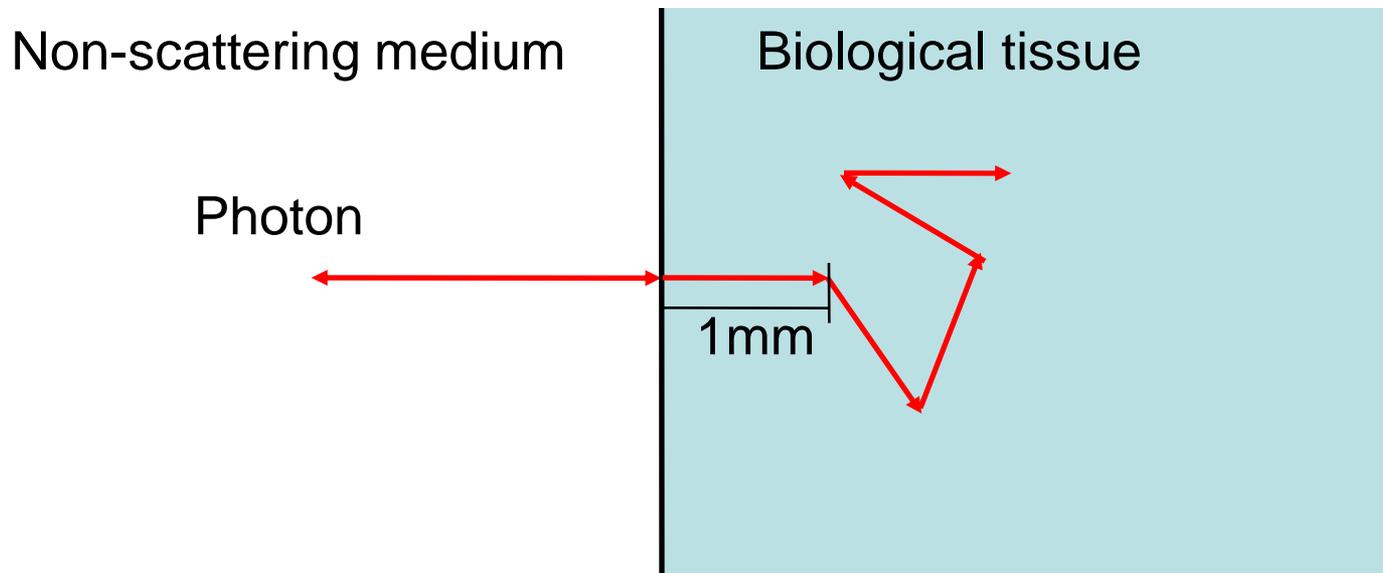


Experimental Techniques

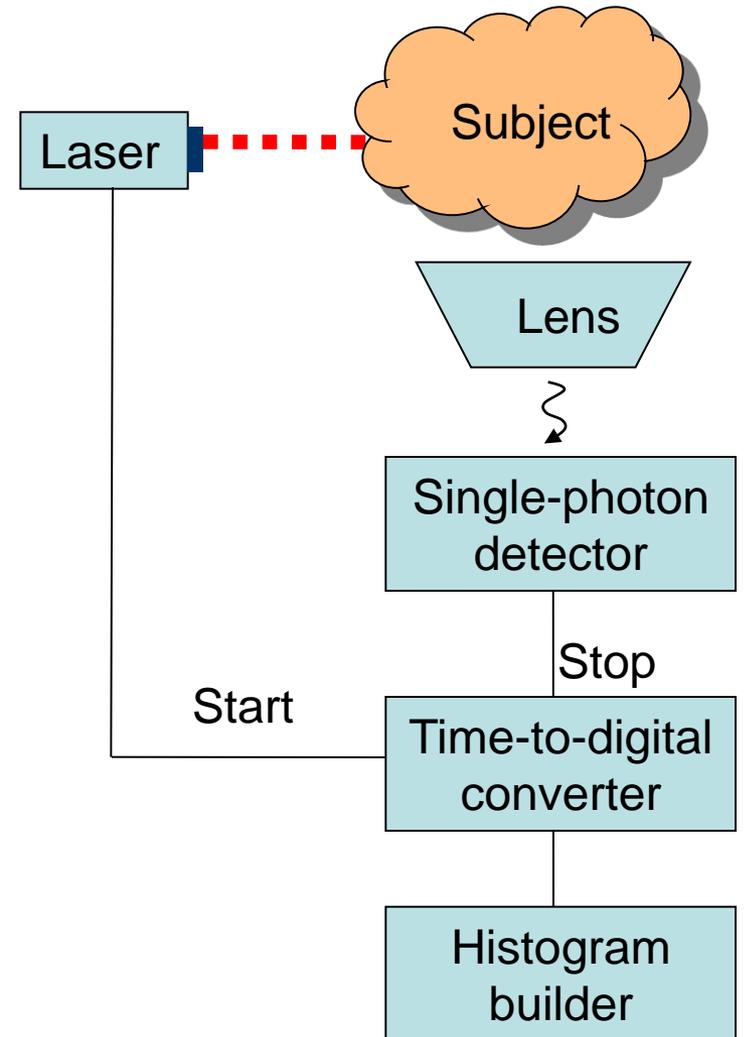
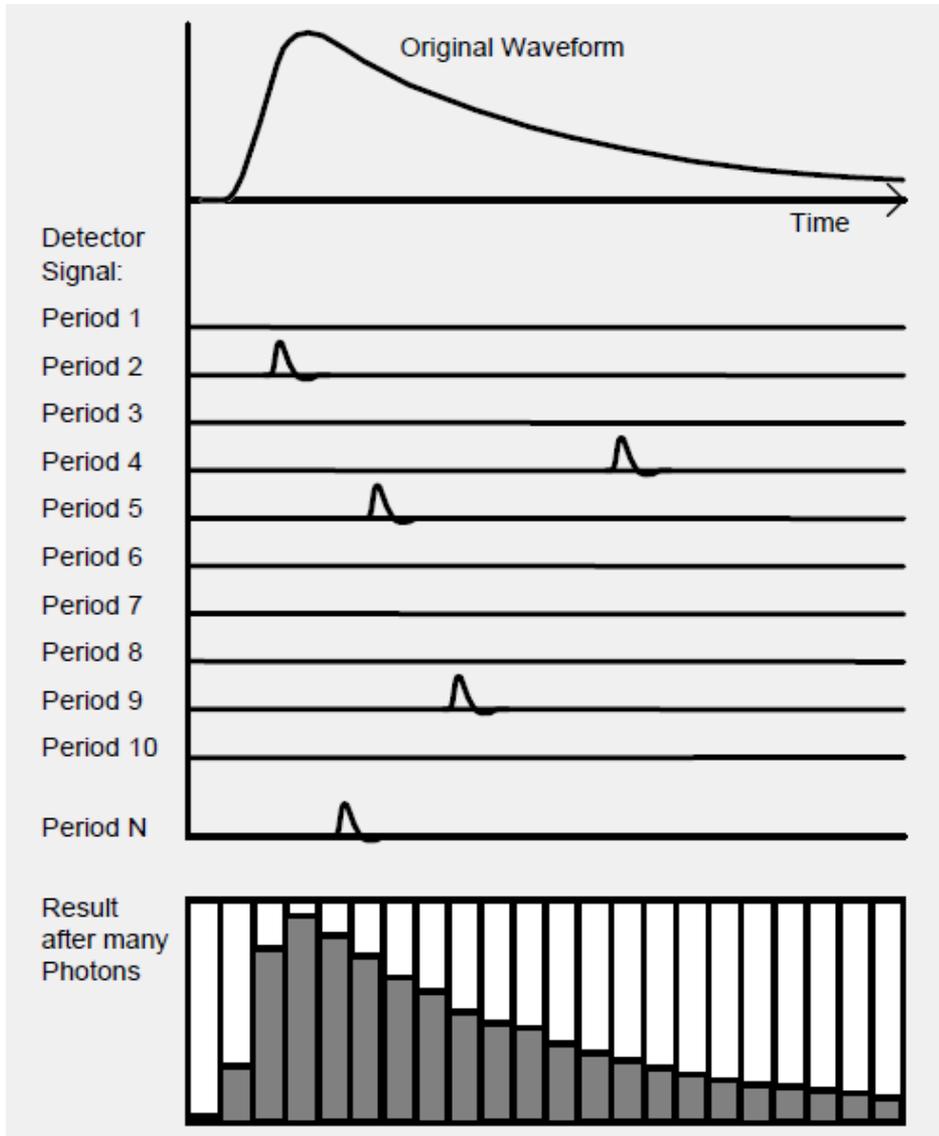


Scattering

- Random walk theory
- Photon random walk step in biological tissue $\sim 1\text{mm}$



Time Correlated Single Photon Counting (TCSPC)

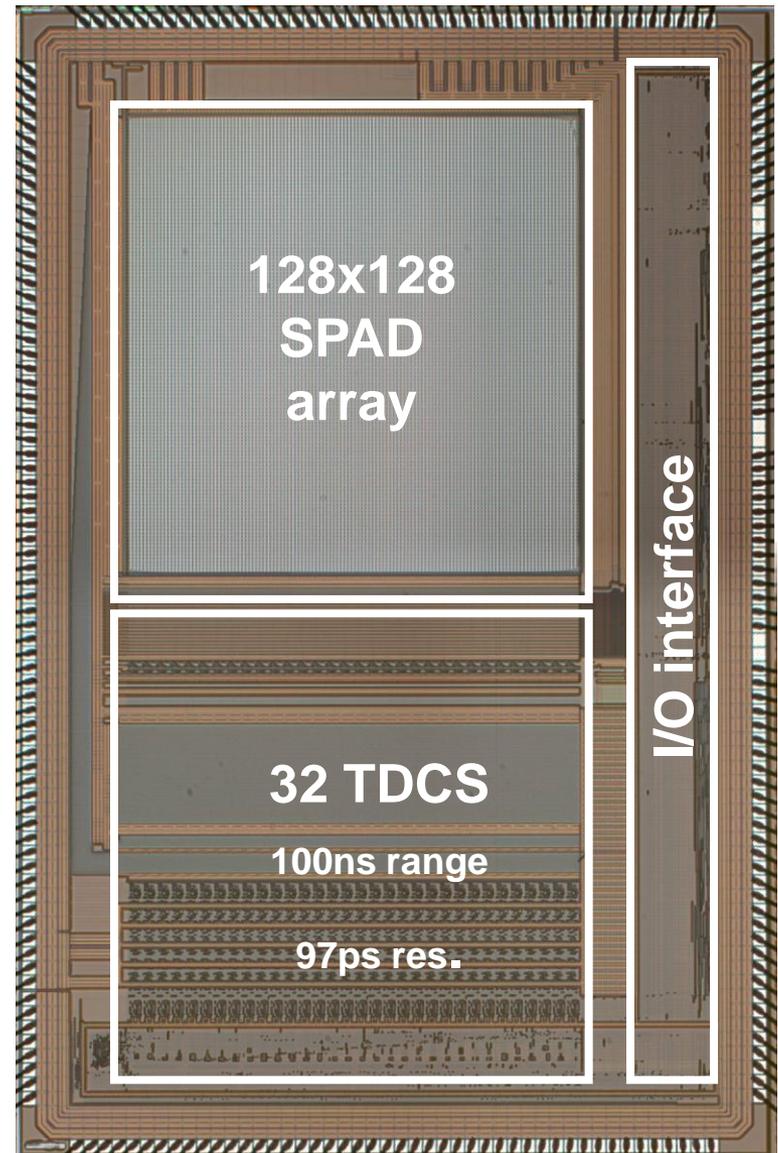
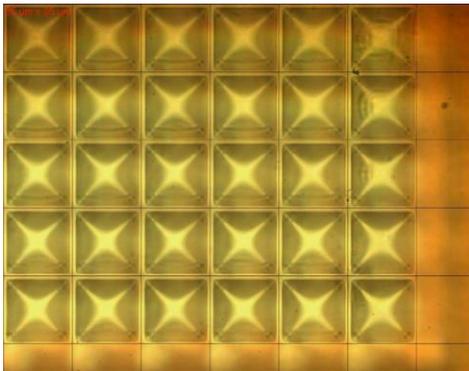


Applications

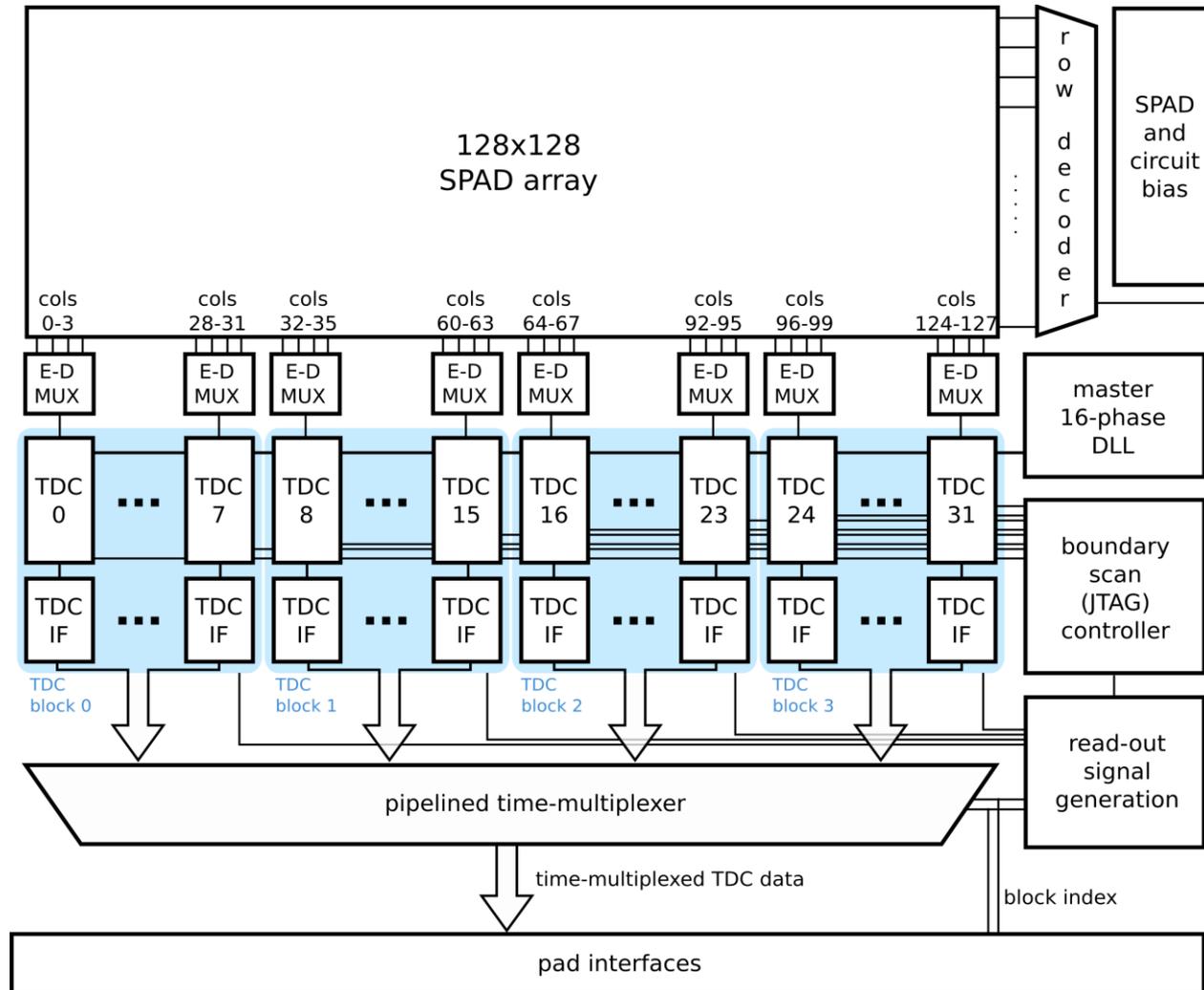
- Perfusion state of tissue
- Tissue oxygenation monitoring
- Internal bleeding
- Detection of infarcts
- Tumor detection and analysis
- Viability of tissue
- Tissue function

SPAD Image Sensor: LASP Chip

- CMOS 0.35 μm technology
- 3.2mm x 3.2mm active area
- Fill factor 6%
- Microlenses improve the fill factor up to 50%



SPAD Image Sensor Architecture



[Niclass et al JSSC 2008]

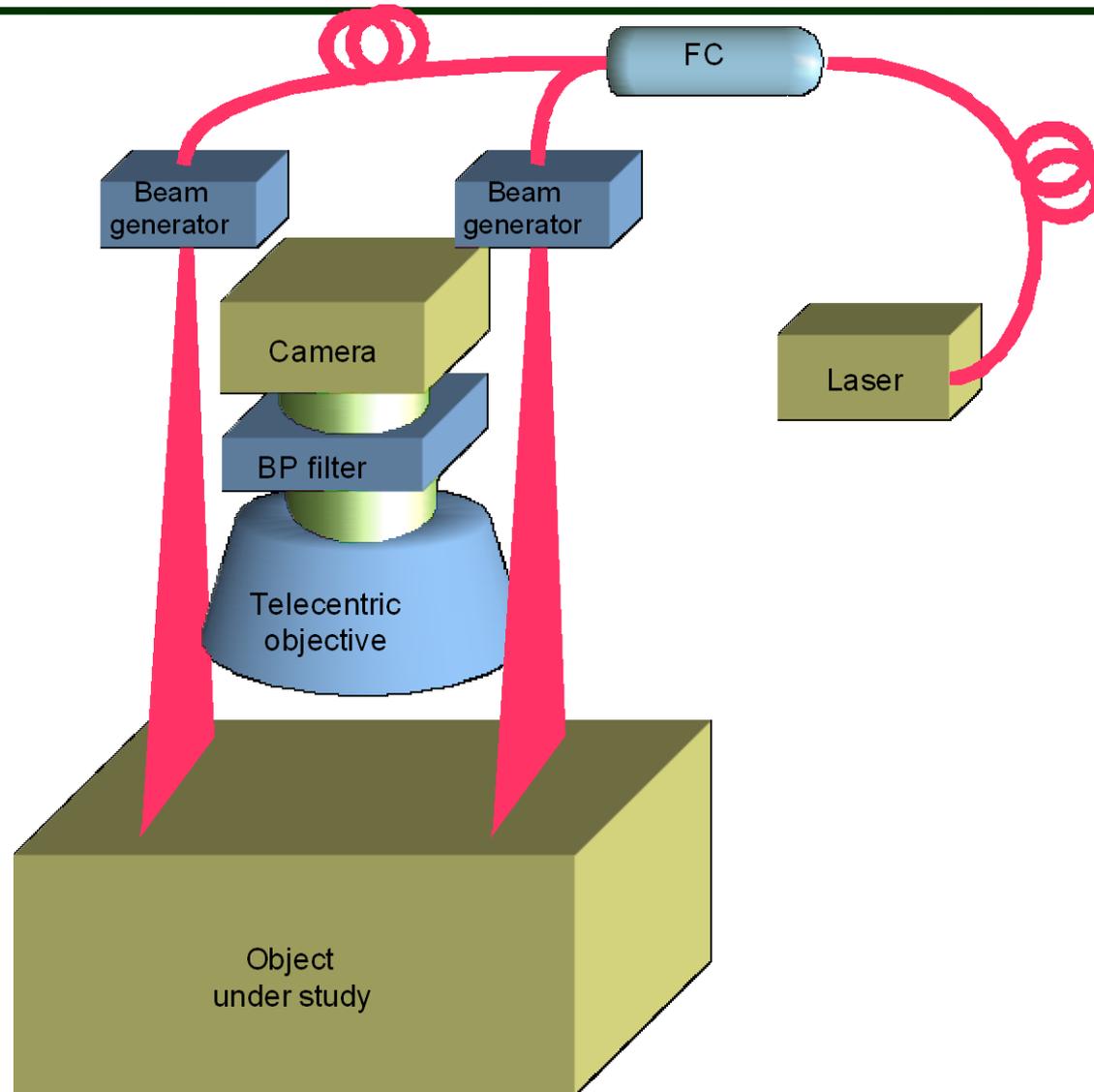
Laser: Becker & Hickl BHL-700

- 780nm wavelength
- Repetition rate 80MHz (fixed)
- Pulse width ~ 100 ps at 1mW
- 0.2mW to 10mW adjustable average CW power
- 300mW typical peak power



[www.becker-hickl.de]

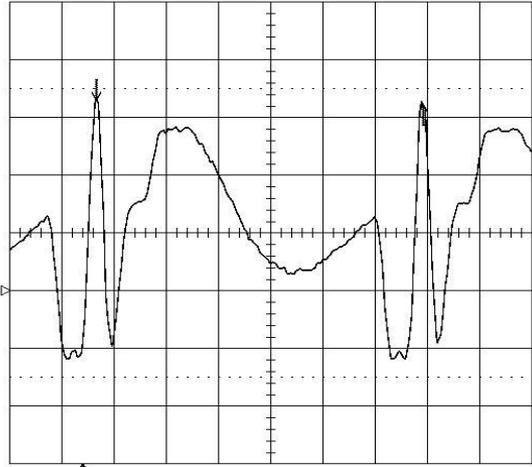
Experimental Setup with Cylindrical Waves I



Trigger Adaptation Circuit

17-Aug-09
12:13:48

2 ns
449 mV
435 mV



MEASURE

OFF **Cursors**
Parameters

mode
Time
Amplitude

type
Relative
Absolute

show
Diff - Ref
Diff & Ref

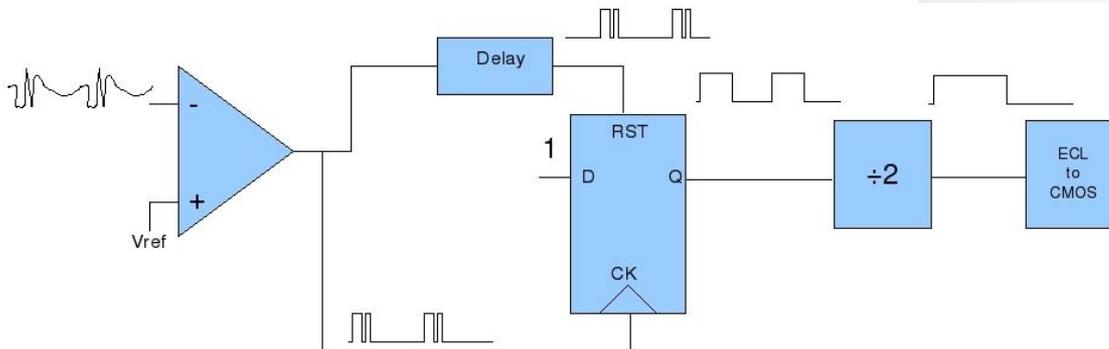
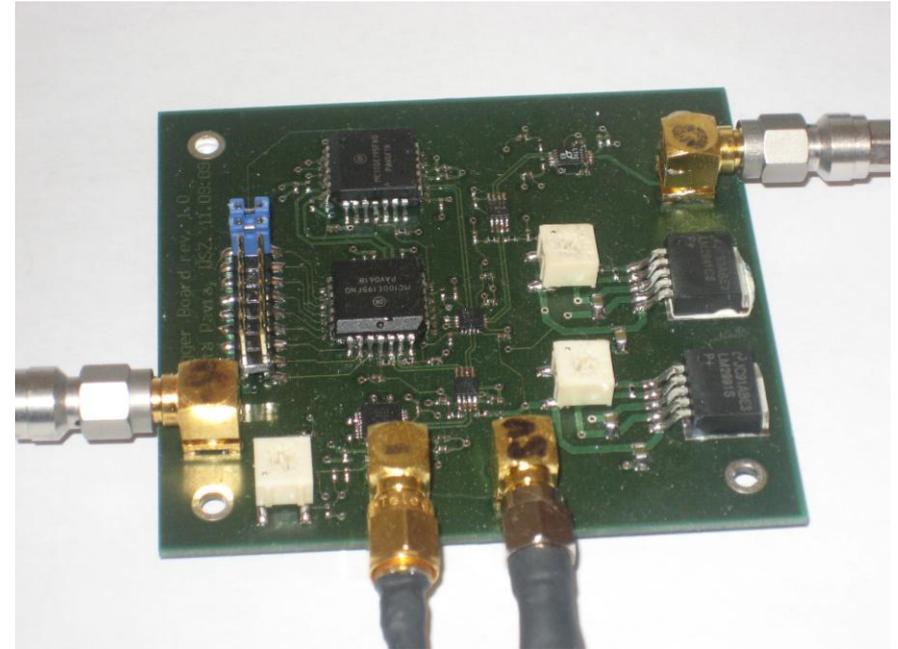
Reference
cursor
Track **OFF** On

Difference
cursor

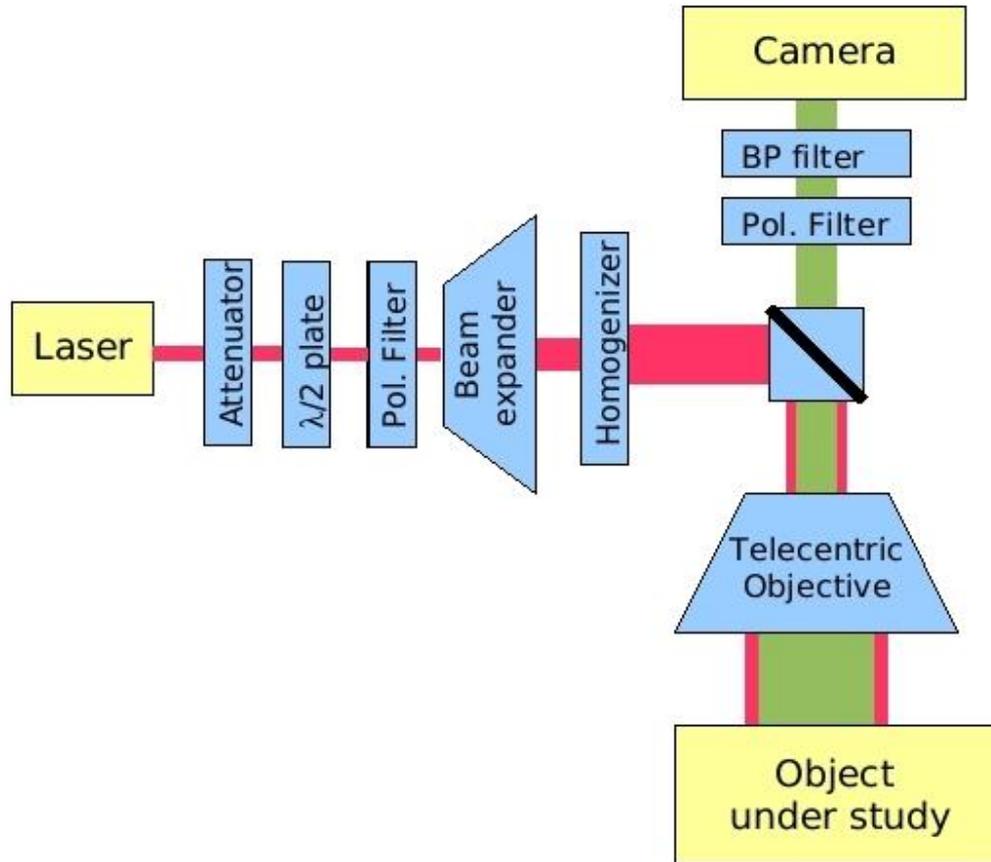
2 ns RIS

1 .2 V 50Ω
2 .5 V DC
3 .5 V DC $\times \frac{\infty}{10}$
4 .5 V DC $\times \frac{\infty}{10}$

Δt 12.50 ns $\frac{1}{2} \Delta t$ 80.00 MHz
10 GS/s
1 DC -0.208 V
□ AUTO

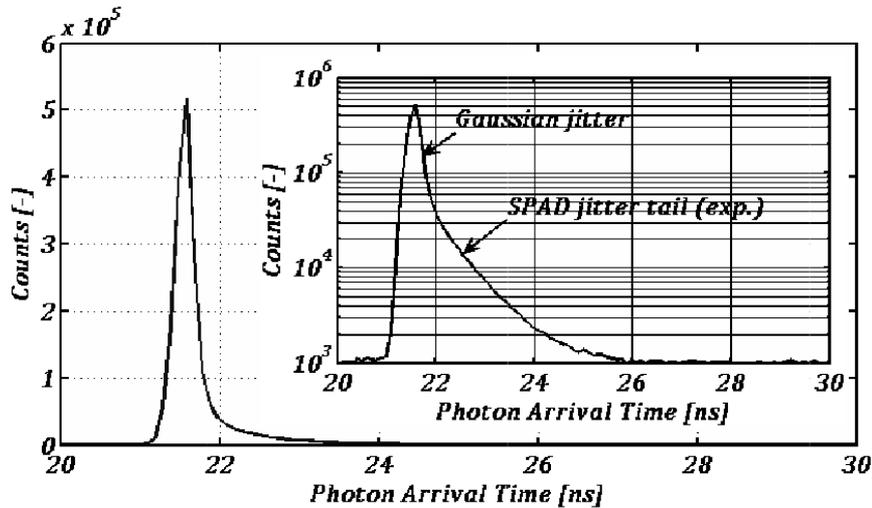


Experimental Setup with Plane Waves

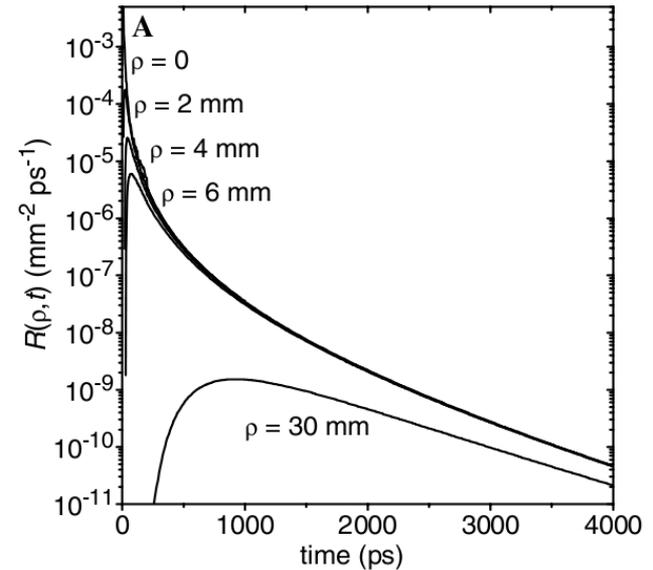


Results with Plane Waves

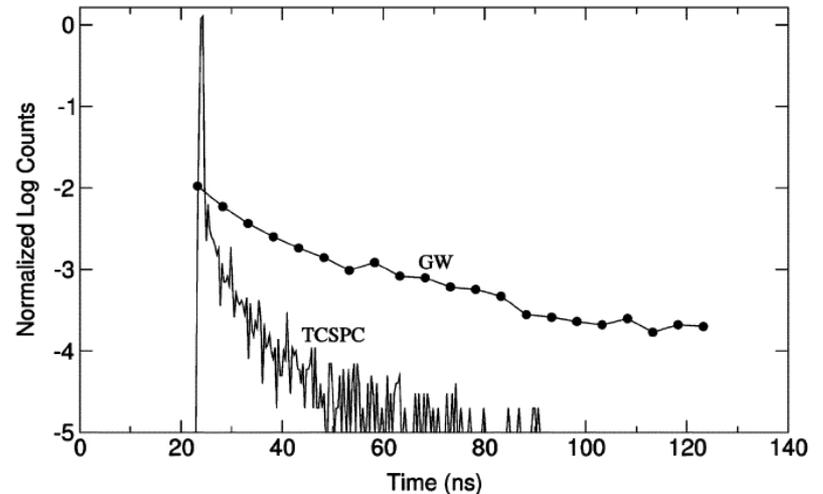
- SPAD's Impulse Response Function (IRF) is too slow
- Time gating-window (GW) does not improve the IRF



[Niclass C et al JSSC 2008]

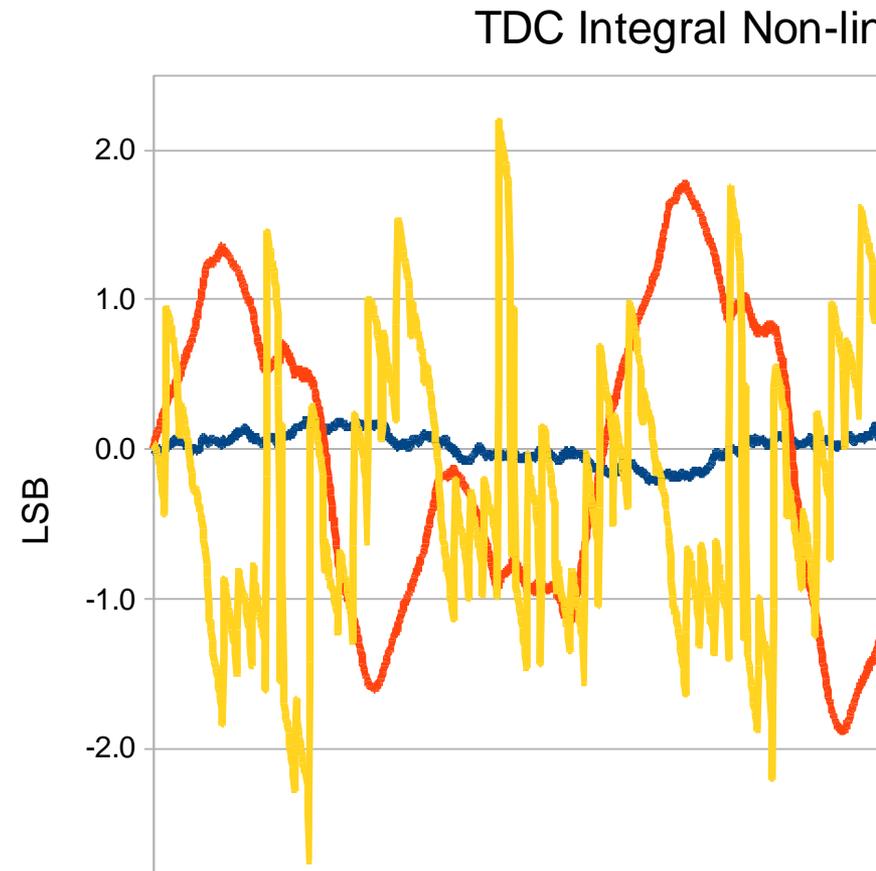
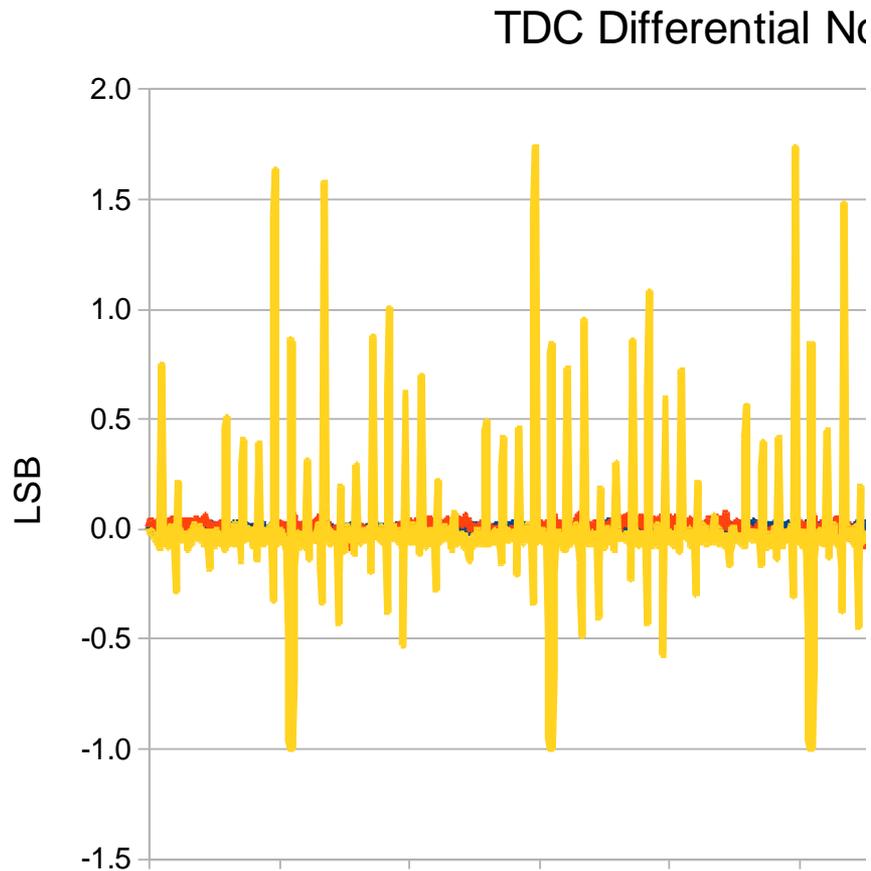


[Torricelli et al. 2005]



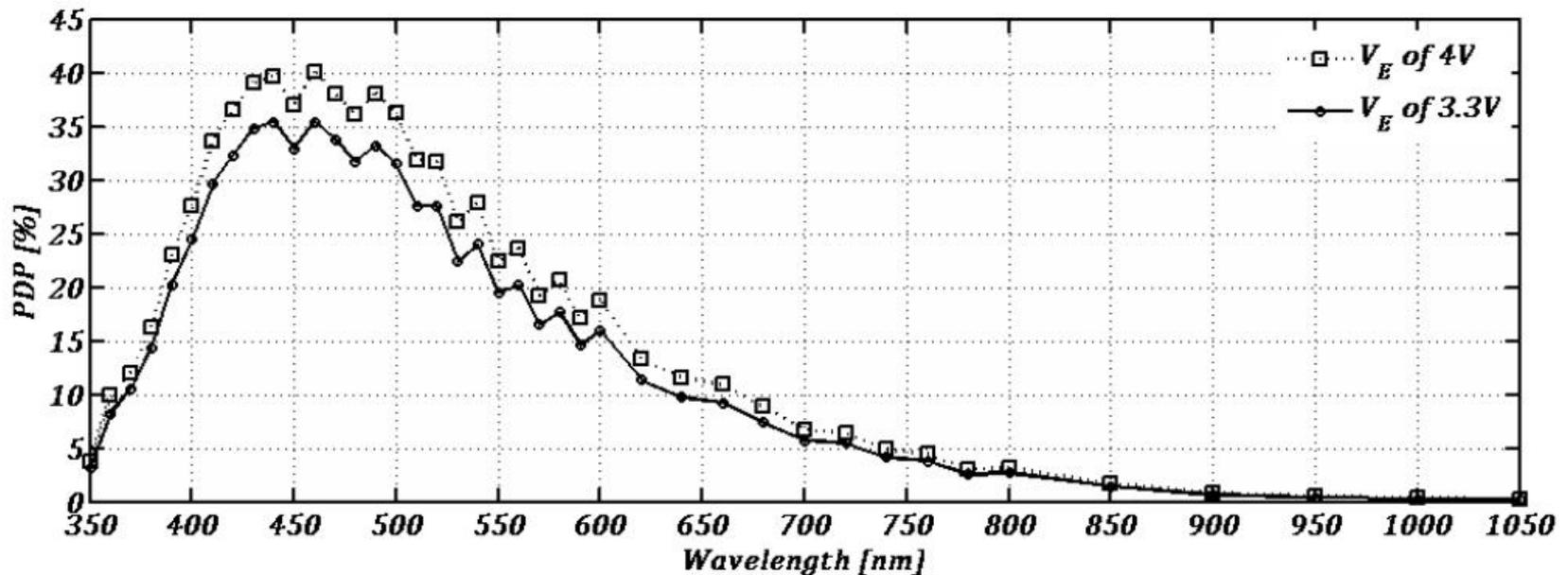
[Schwartz D et al JSSC 2008]

Time-to-digital Converter Linearity



Detector: Photon Detection Probability (PDP)

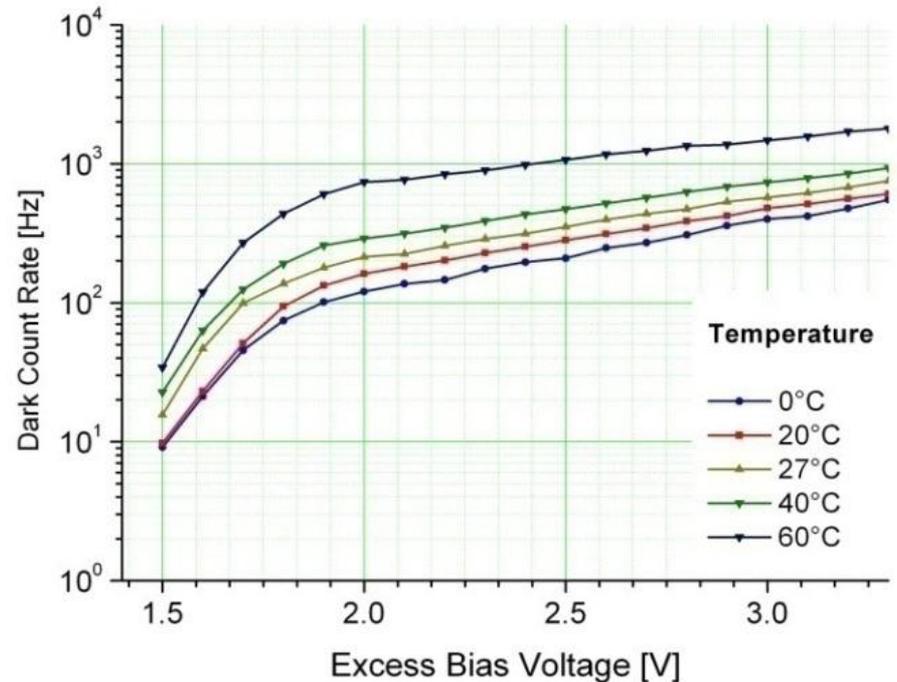
- PDP increases with the excess bias voltage, but so does the DCR.
- The shallow p+ / n-well junction explains why the SPAD is more effective at blue/UV wavelengths than at red/IR.



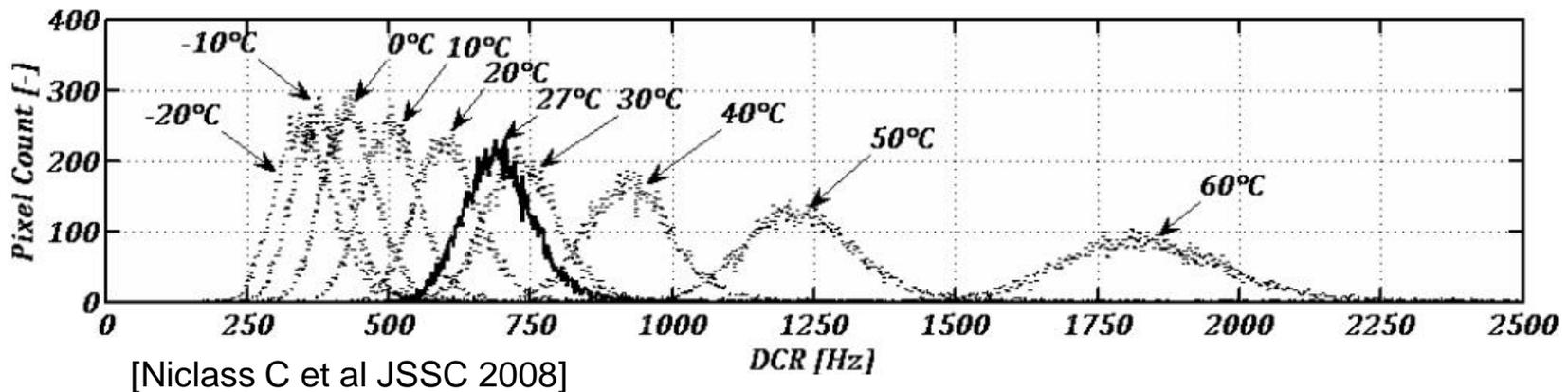
[Niclass C et al JSSC 2008]

Dark Count Rate (DCR)

- Pulses generated in the SPAD in the absence of light.
- Causes:
 - Thermal generation of carriers
 - Electron-hole generation due to tunneling effects.

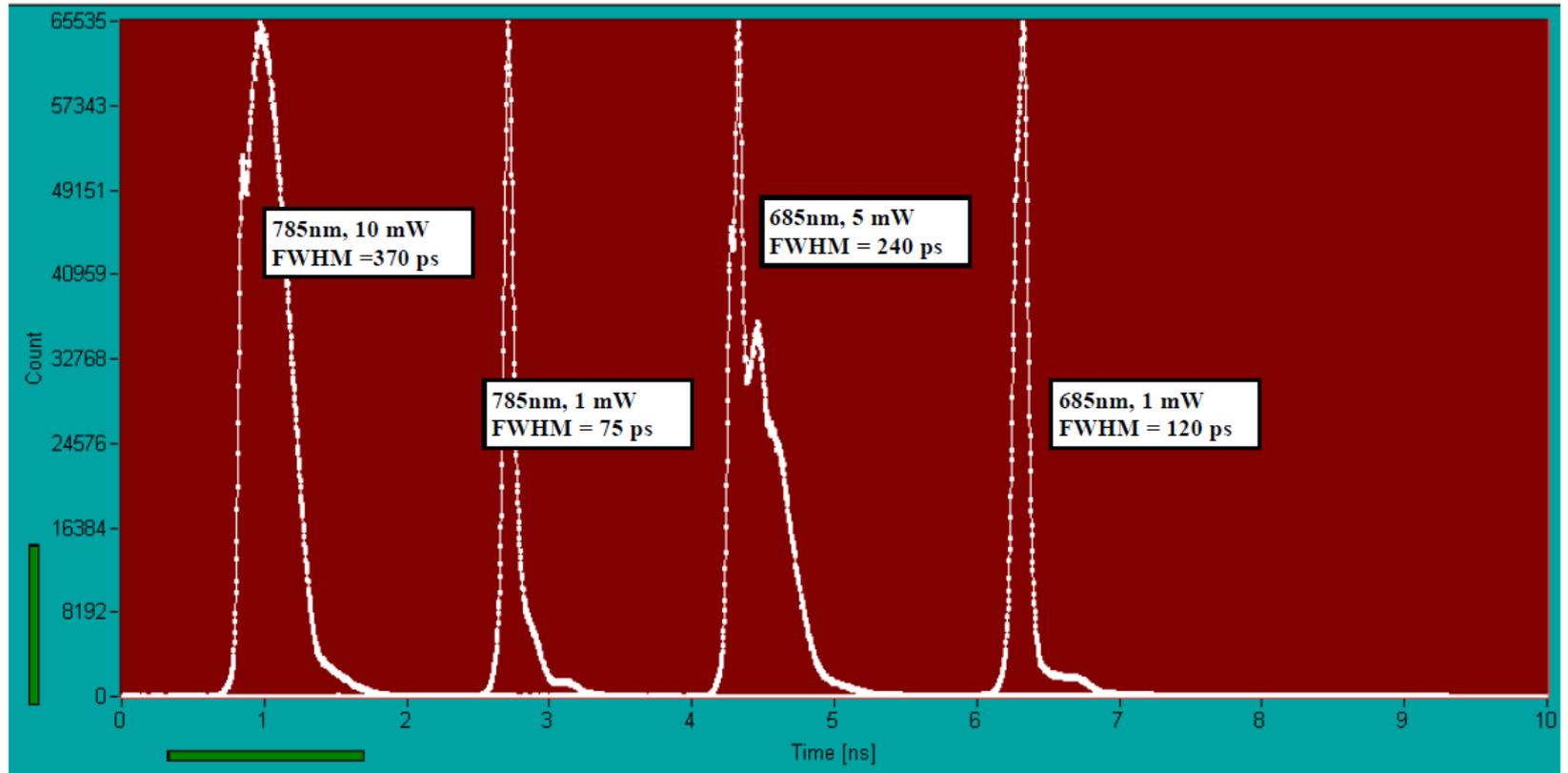


[Niclass C et al JSSC 2008]



[Niclass C et al JSSC 2008]

BHP-700 time response



The Diffusion Equation

- Homogeneous medium
- Fourier in the time domain

$$\frac{\partial U(\vec{r}, t)}{\partial t} + v\mu_a U(\vec{r}, t) + \nabla \cdot \vec{J}(\vec{r}, t) = q(\vec{r}, t)$$

$$\nabla U(\vec{r}, t) + \frac{3\partial \vec{J}(\vec{r}, t)}{v^2 \partial t} + \frac{\vec{J}(\vec{r}, t)}{D} = 0$$

$$D = \frac{v}{3\mu'_s}$$

$U(\vec{r}, t)$: photon density wave

$\vec{J}(\vec{r}, t)$: photon density current

v : speed of light

μ_a : absorption coefficient

μ'_s : reduced scattering coefficient

D : diffusion coefficient

$q(\vec{r}, t)$: source term

$$\nabla^2 U(\vec{r}, \omega_t) + k^2 U(\vec{r}, \omega_t) = -\frac{q(\vec{r}, \omega_t)}{D}$$

$$k^2 = \frac{(-v\mu_a - i\omega_t)}{D}$$

Using the first Born approximation

$$\mu_a(\vec{r}) = \mu_a^0 + \mu_a^s(\vec{r}) \quad U(\vec{r}) = U_0(\vec{r}) + U_s(\vec{r})$$

$$(\nabla^2 + k^2)U_s(\vec{r}) = \frac{v\mu_a^s(\vec{r})}{D}(U_0(\vec{r}) + U_s(\vec{r}))$$

Object to be reconstructed

$$U_s(\vec{r}) = - \int g(\vec{r}|\vec{r}') \frac{v\mu_a^s(\vec{r}')}{D} U_0(\vec{r}') d\vec{r}'$$

Measurement Matrix coefficients

The Diffusion Equation for Plane Waves

Fourier in XY dimensions

$$\left(\frac{\partial^2}{\partial z^2} + (k^2 - \omega_x^2 - \omega_y^2)\right)U_s(\omega_x, \omega_y, z) = \mathcal{F}_{xy} \left\{ \frac{v\mu_a^s(\vec{r}')}{D} U_0(\vec{r}') \right\}$$

$$\gamma_{xy}^2 = \omega_x^2 + \omega_y^2 - k^2$$

Infinite medium

$$U_s(\omega_x, \omega_y, z) = - \int \mathcal{F}_{xy} \left\{ \frac{v\mu_a^s(\vec{r}')}{D} U_0(\vec{r}') \frac{e^{-\gamma_{xy}|z-z'|}}{2\gamma_{xy}} dz' \right\}$$

Homogeneous field is XY independent

$$U_s(\omega_x, \omega_y, z) = -\frac{ie^{-\gamma_{xy}z+ikz_0}}{4Dk\gamma_{xy}} \int O(\omega_x, \omega_y, z')e^{(\gamma_{xy}-ik)z'} dz'; o(\vec{r}) = \frac{v\mu_a^s(\vec{r}')}{D}$$

The Diffusion Equation for Cylindrical Waves

Fourier in the X dimension

$$\left(\frac{\partial^2}{\partial z^2} + \frac{\partial^2}{\partial x^2} + (k^2 - \omega_x^2)\right)U_s(\omega_x, y, z) = \mathcal{F}_x\left\{\frac{v\mu_a^s(\vec{r}')}{D}U_0(\vec{r}')\right\}$$

$$\gamma_x^2 = \omega_x^2 - k^2$$

Infinite medium

$$U_s(\omega_x, y, z) = - \iint \mathcal{F}_x\left\{\frac{v\mu_a^s(\vec{r}')}{D}U_0(\vec{r}')\right\} \frac{i}{4}H_0^{(1)}(i\gamma_x|\vec{r}'_{yz} - \vec{r}_{yz}^0|) dy' dz'$$

Homogeneous field is X independent

$$U_s(\omega_x, y, z) = - \iint O(\omega_x, y', z') \frac{i}{4D}H_0^{(1)}(k|\vec{r}'_{yz} - \vec{r}_{yz}^0|) \frac{i}{4}H_0^{(1)}(i\gamma_x|\vec{r}'_{yz} - \vec{r}'_{yz}|) dy' dz'$$

Reconstruction Algorithm

- **Semi-infinite medium:** the method of images can be applied
- **Multiple sources:** superposition principle
- **TD measurements:** high number of equations for only one acquisition

The Inverse Problem: Regularization

- The problem is ill-posed by its nature.
- Regularization defines restrictions in the solution's complexity: smoothness, norm ...
- Tikhonov regularization: equivalent to minimize:
- Sub-space preconditioned LSQR (SP-LSQR):
 - Iterative method
 - Tikhonov regularization
 - Predefined sub-space of possible solutions

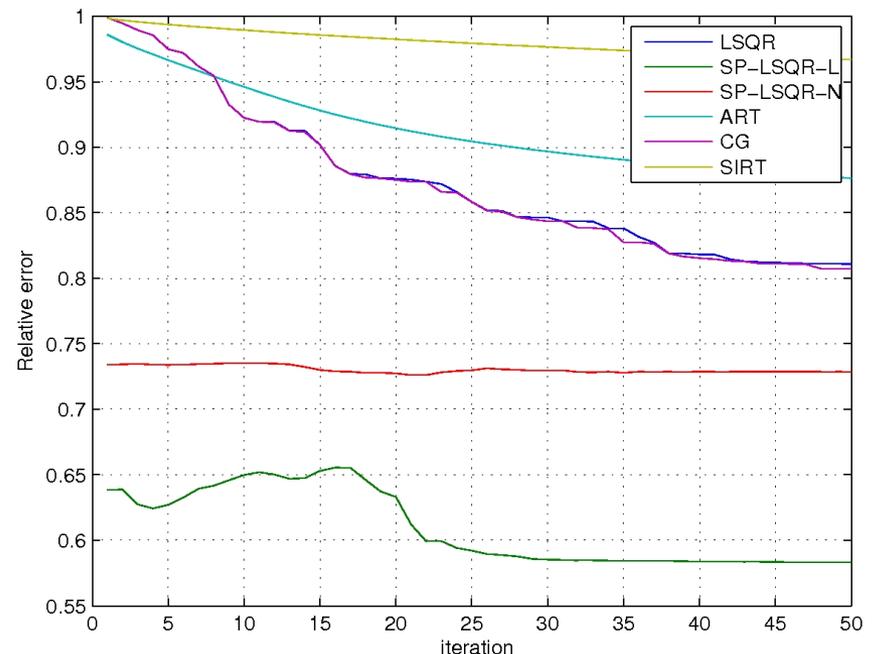
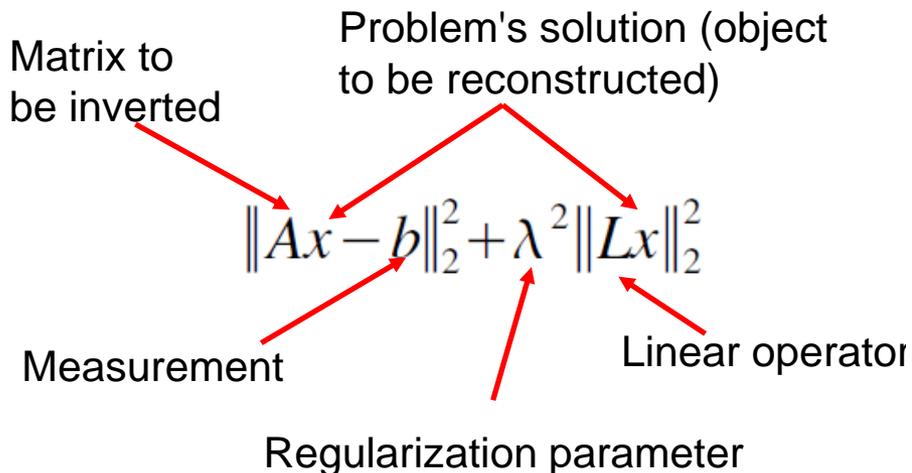
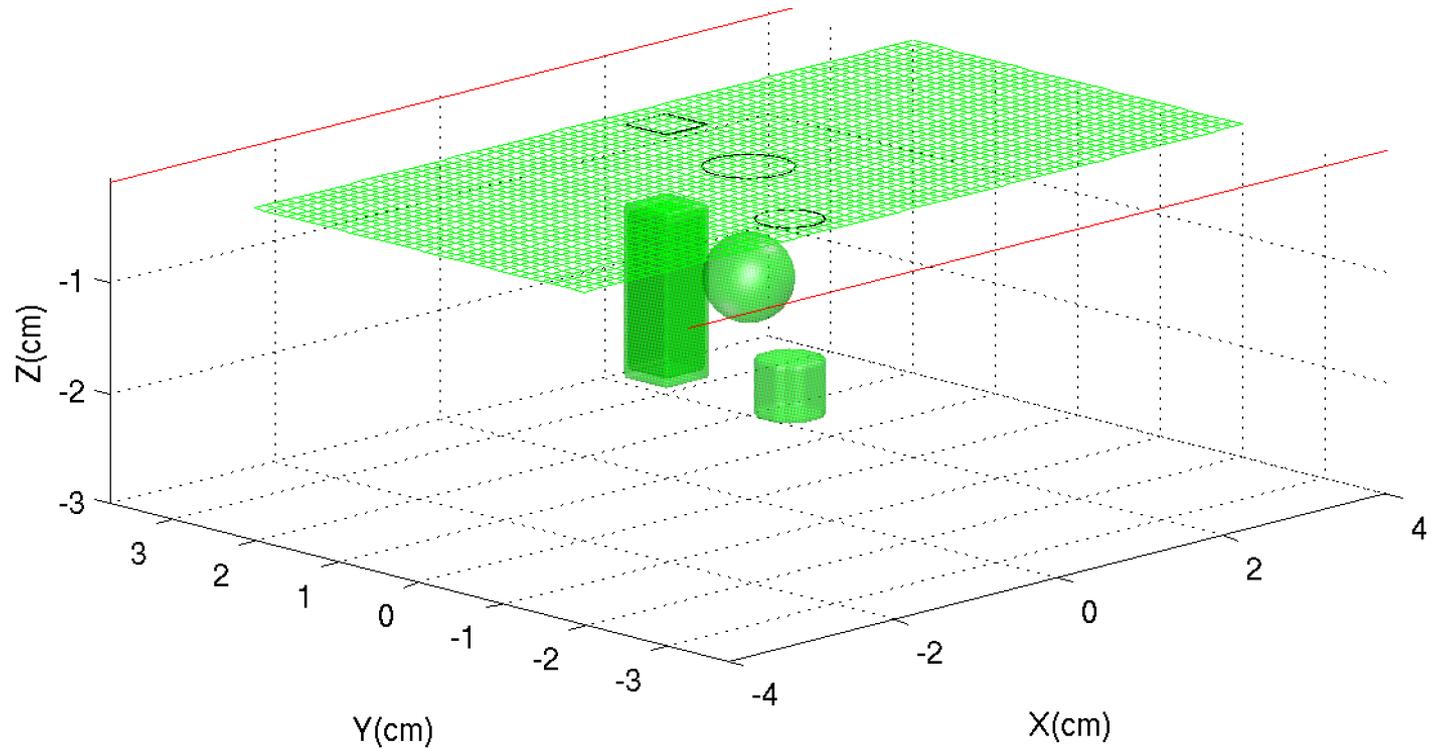
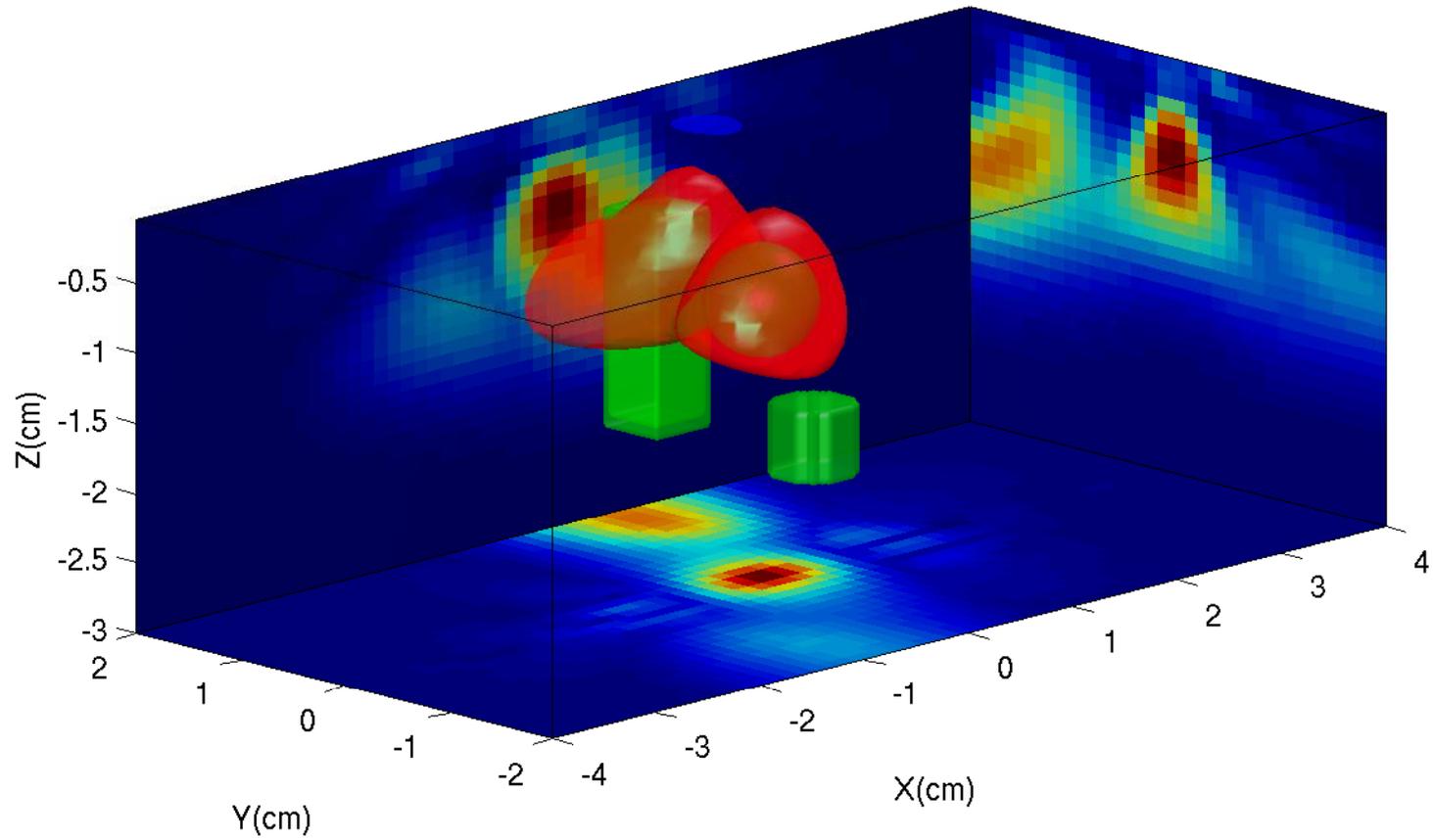


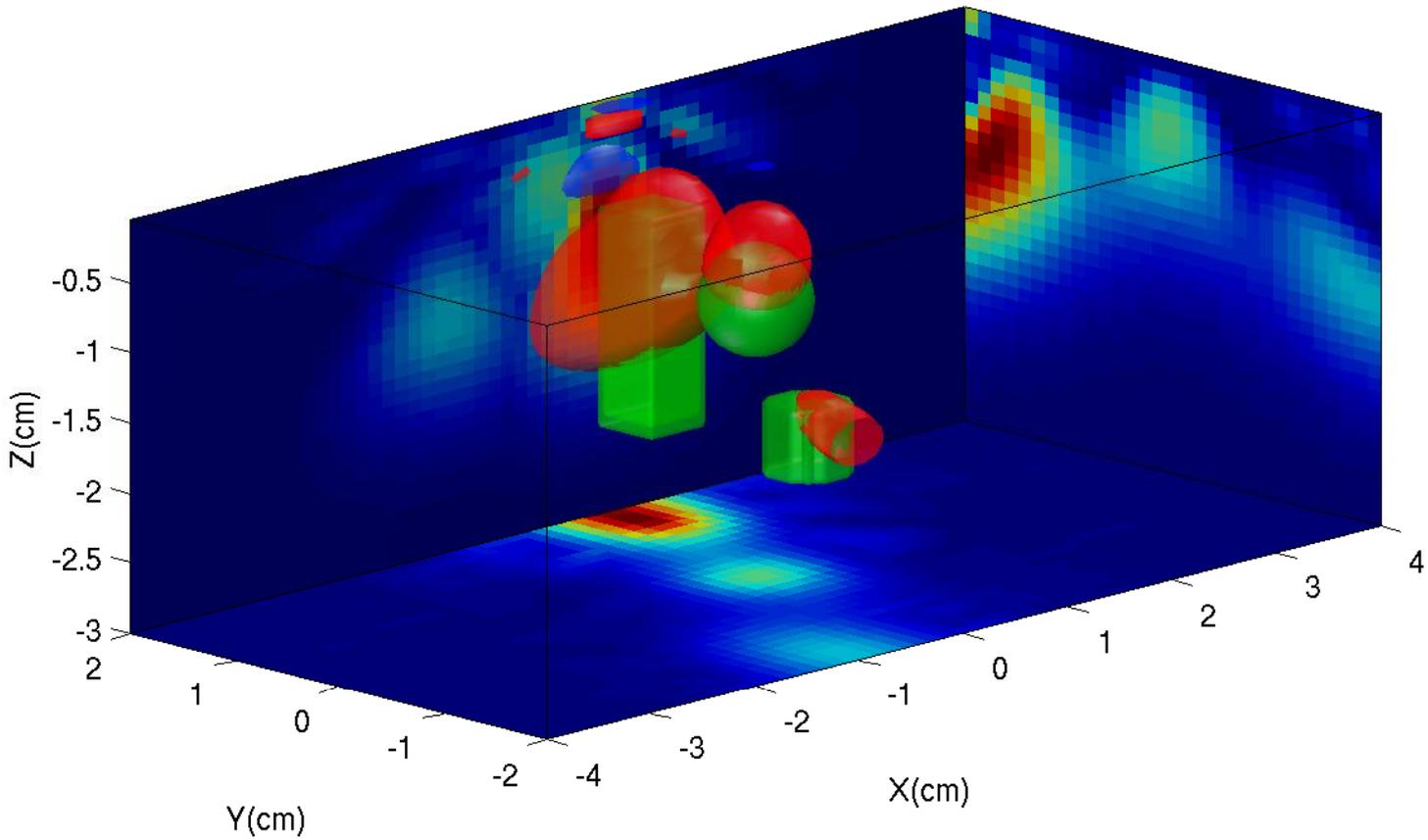
Image Reconstruction Testbench



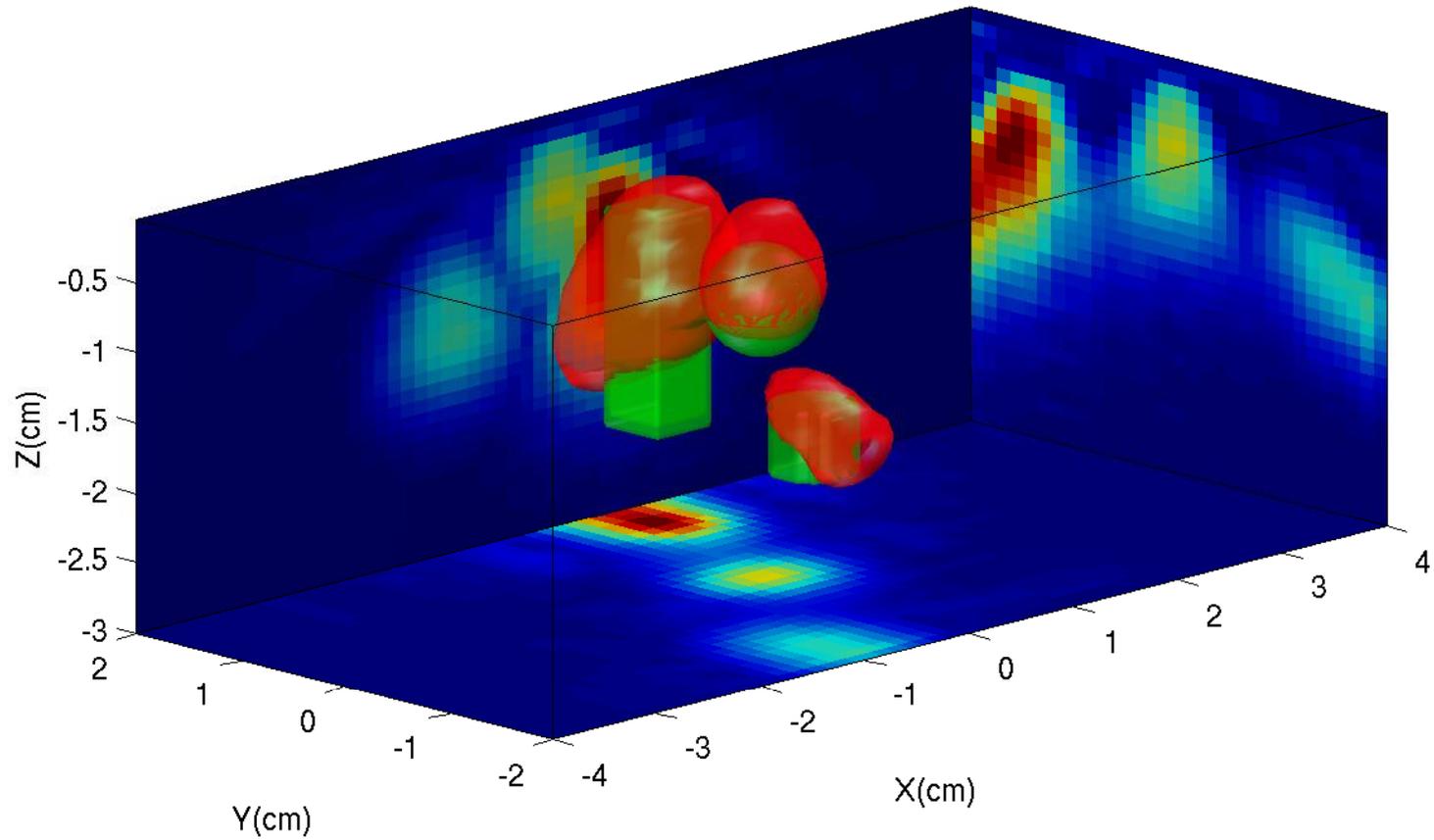
Simulation Results: ART



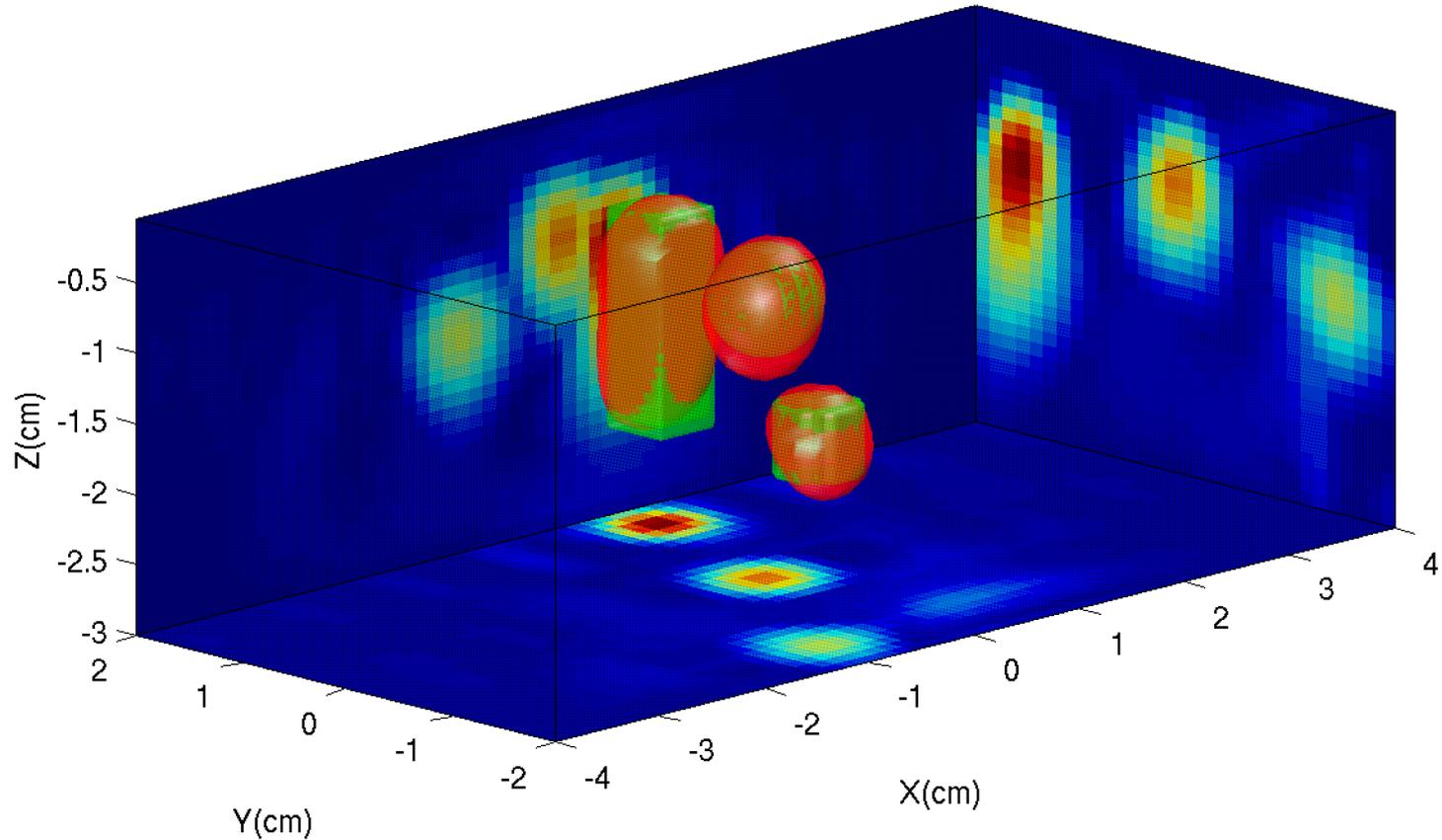
Simulation Results: LSQR



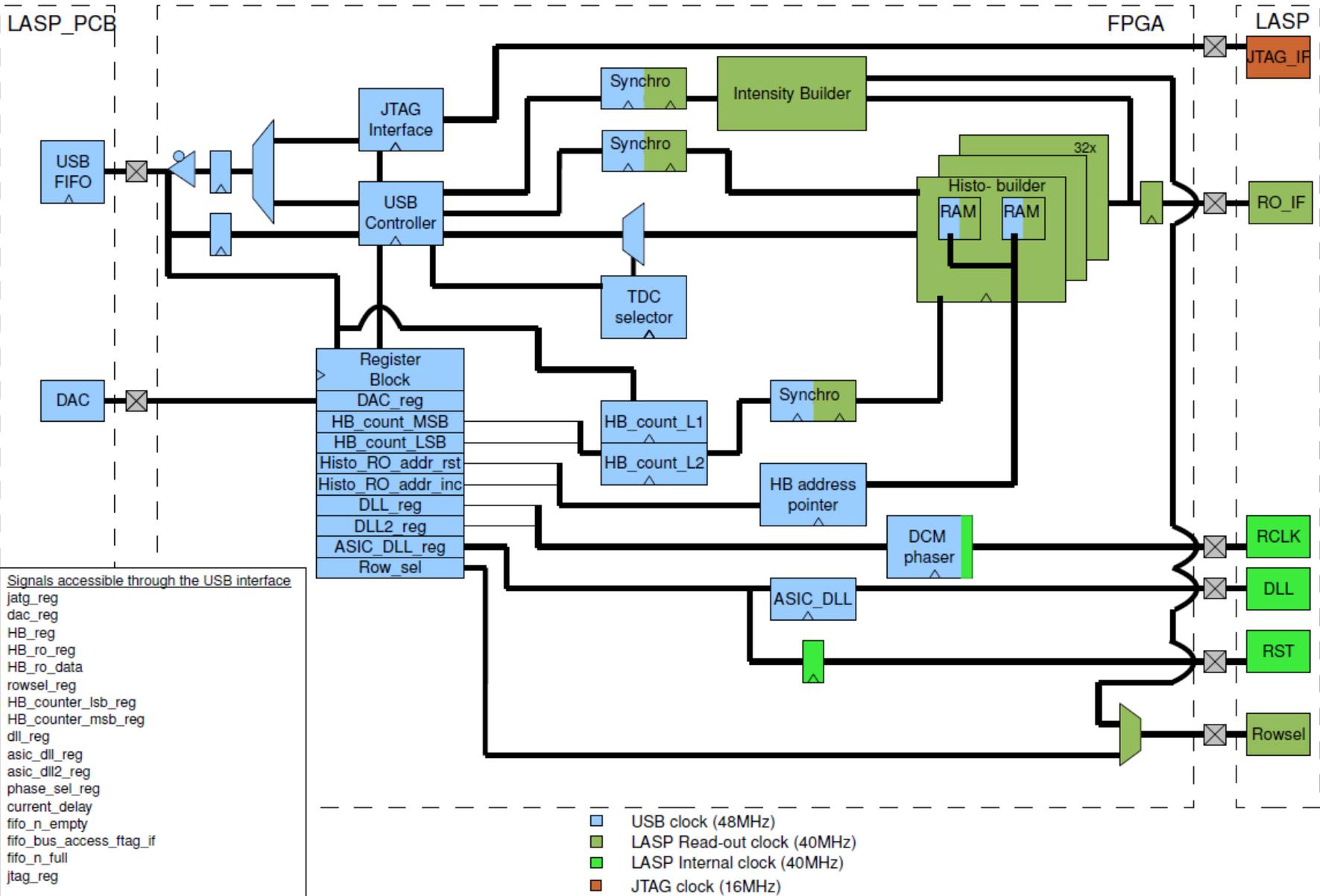
Simulation Results: SP-LSQR Norm



Simulation Results with SP-LSQR

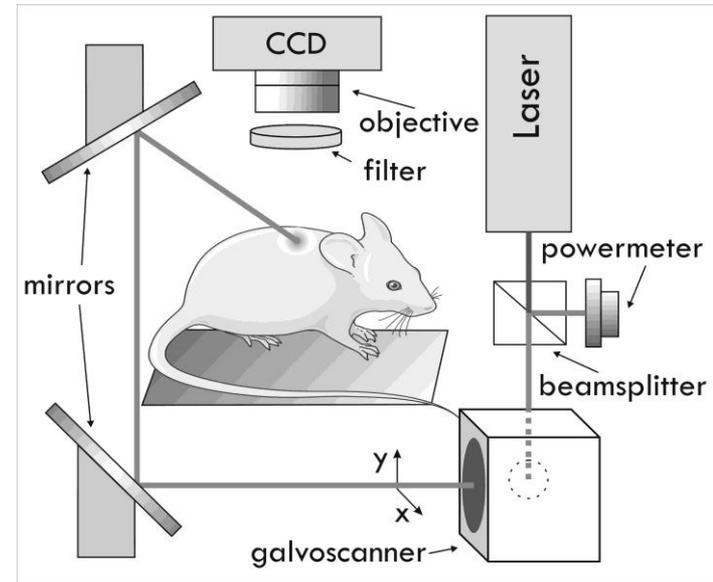


FPGA Architecture for fast data acquisition

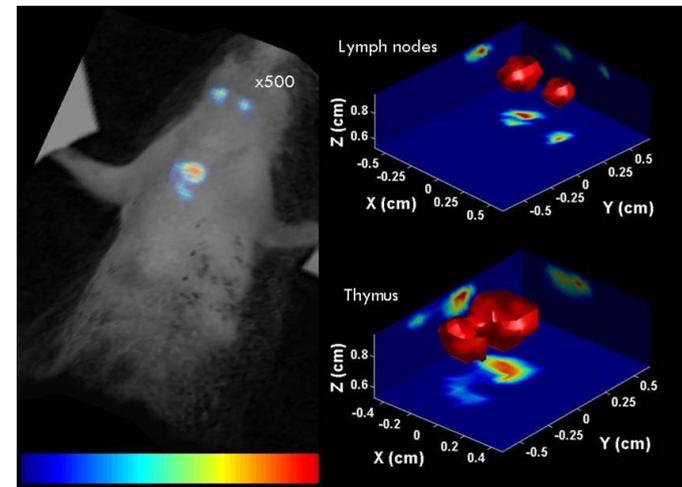


High definition imaging with NIR

- CW systems with CCD cameras.
- Long acquisition times: Full scan of the object.
- Low depth resolution.
- Only applied to small spaces. E.g. small animal imaging.



[A. Martin, Mol. Img. (2008)]



[A. Martin, Mol. Img. (2009)]

Future Modifications of the SPAD Image Sensor

- Solve the Linearity problem in the TDC
- Reduce the total time range of the TDC
- Increase the number of pixels
- Modify the TDC/pixel clustering to reduce the number of acquisitions per frame

Outlook

- ✓ Design a NIRI system based on a SPAD image sensor
- ✓ Develop an image reconstruction algorithm based on the system
- ✓ Build a system to perform measurements on phantoms
- Evaluate the performance of the new setup
 - Design a customized SPAD image sensor
 - Pre-clinical trials

Conclusions

- SPADs enable the acquisition of time-resolved measurements with high spatial resolution for NIRI
- They make possible the development of more efficient algorithms:
 - Higher resolution images
 - Less computation power